



## SERIES “ATS/ERS TASK FORCE: STANDARDISATION OF LUNG FUNCTION TESTING”

Edited by V. Brusasco, R. Crapo and G. Viegi  
Number 2 in this Series

# Standardisation of spirometry

M.R. Miller, J. Hankinson, V. Brusasco, F. Burgos, R. Casaburi, A. Coates,  
R. Crapo, P. Enright, C.P.M. van der Grinten, P. Gustafsson, R. Jensen,  
D.C. Johnson, N. MacIntyre, R. McKay, D. Navajas, O.F. Pedersen, R. Pellegrino,  
G. Viegi and J. Wanger

### CONTENTS

<b>Background</b> . . . . .	320
<b>FEV<sub>1</sub> and FVC manoeuvre</b> . . . . .	321
Definitions . . . . .	321
Equipment . . . . .	321
Requirements . . . . .	321
Display . . . . .	321
Validation . . . . .	322
Quality control . . . . .	322
Quality control for volume-measuring devices . . . . .	322
Quality control for flow-measuring devices . . . . .	323
Test procedure . . . . .	323
Within-manoeuve evaluation . . . . .	324
Start of test criteria . . . . .	324
End of test criteria . . . . .	324
Additional criteria . . . . .	324
Summary of acceptable blow criteria . . . . .	325
Between-manoeuve evaluation . . . . .	325
Manoeuvre repeatability . . . . .	325
Maximum number of manoeuvres . . . . .	326
Test result selection . . . . .	326
Other derived indices . . . . .	326
FEV <sub>t</sub> . . . . .	326
Standardisation of FEV <sub>1</sub> for expired volume, FEV <sub>1</sub> /FVC and FEV <sub>1</sub> /VC . . . . .	326
FEF <sub>25–75%</sub> . . . . .	326
PEF . . . . .	326
Maximal expiratory flow–volume loops . . . . .	326
Definitions . . . . .	326
Equipment . . . . .	327
Test procedure . . . . .	327
Within- and between-manoeuve evaluation . . . . .	327
Flow–volume loop examples . . . . .	327
Reversibility testing . . . . .	327
Method . . . . .	327
Comment on dose and delivery method . . . . .	328
Determination of reversibility . . . . .	328
<b>VC and IC manoeuvre</b> . . . . .	329
Definitions . . . . .	329

### AFFILIATIONS

For affiliations, please see  
Acknowledgements section

### CORRESPONDENCE

V. Brusasco  
Internal Medicine  
University of Genoa  
V.le Benedetto XV, 6  
I-16132 Genova  
Italy  
Fax: 39 103537690  
E-mail: vito.brusasco@unige.it

### Received:

March 23 2005

### Accepted after revision:

April 05 2005

**Previous articles in this series: No. 1:** Miller MR, Crapo R, Hankinson J, *et al.* General considerations for lung function testing. *Eur Respir J* 2005; 26: 153–161.

European Respiratory Journal  
Print ISSN 0903-1936  
Online ISSN 1399-3003

VC and IVC . . . . .	329	Test procedure . . . . .	331
IC . . . . .	329	Within-manoeuvre evaluation . . . . .	331
Equipment . . . . .	329	Between-manoeuvre evaluation . . . . .	331
Test procedure . . . . .	329	Test result selection . . . . .	331
VC . . . . .	329	<b>Technical considerations</b> . . . . .	331
IC . . . . .	330	Minimal recommendations for spirometry systems . . . . .	331
Use of a nose clip . . . . .	330	BTPS correction . . . . .	332
Within-manoeuvre evaluation . . . . .	330	Comments . . . . .	332
Between-manoeuvre evaluation . . . . .	330	Test signals for spirometer testing . . . . .	333
Test result selection . . . . .	330	Method . . . . .	333
<b>Peak expiratory flow</b> . . . . .	330	Accuracy test . . . . .	333
Definition . . . . .	330	Repeatability test . . . . .	333
Equipment . . . . .	330	Test signals for PEF meter testing . . . . .	333
Test procedure . . . . .	330	Method . . . . .	333
Within-manoeuvre evaluation . . . . .	331	Accuracy test . . . . .	333
Between-manoeuvre evaluation . . . . .	331	Repeatability test . . . . .	334
Test result selection . . . . .	331	Test signals for MVV testing . . . . .	334
<b>Maximum voluntary ventilation</b> . . . . .	331	<b>Abbreviations</b> . . . . .	334
Definition . . . . .	331	<b>Appendix</b> . . . . .	335
Equipment . . . . .	331		

**KEYWORDS:** Peak expiratory flow, spirometry, spirometry standardisation, spirometry technique, spirometry training, ventilation

## BACKGROUND

Spirometry is a physiological test that measures how an individual inhales or exhales volumes of air as a function of time. The primary signal measured in spirometry may be volume or flow.

Spirometry is invaluable as a screening test of general respiratory health in the same way that blood pressure provides important information about general cardiovascular health. However, on its own, spirometry does not lead clinicians directly to an aetiological diagnosis. Some indications for spirometry are given in table 1.

In this document, the most important aspects of spirometry are the forced vital capacity (FVC), which is the volume delivered during an expiration made as forcefully and completely as possible starting from full inspiration, and the forced expiratory volume (FEV) in one second, which is the volume delivered in the first second of an FVC manoeuvre. Other spirometric variables derived from the FVC manoeuvre are also addressed.

Spirometry can be undertaken with many different types of equipment, and requires cooperation between the subject and the examiner, and the results obtained will depend on technical as well as personal factors (fig. 1). If the variability of the results can be diminished and the measurement accuracy can be improved, the range of normal values for populations can be narrowed and abnormalities more easily detected. The Snowbird workshop held in 1979 resulted in the first American Thoracic Society (ATS) statement on the standardisation of spirometry [1]. This was updated in 1987 and again in 1994 [2, 3]. A similar initiative was undertaken by the European Community for Steel and Coal, resulting in the first European standardisation document in 1983 [4]. This was

then updated in 1993 as the official statement of the European Respiratory Society (ERS) [5]. There are generally only minor differences between the two most recent ATS and ERS statements, except that the ERS statement includes absolute lung volumes and the ATS does not.

This document brings the views of the ATS and ERS together in an attempt to publish standards that can be applied more

**TABLE 1** Indications for spirometry

### Diagnostic

- To evaluate symptoms, signs or abnormal laboratory tests
- To measure the effect of disease on pulmonary function
- To screen individuals at risk of having pulmonary disease
- To assess pre-operative risk
- To assess prognosis
- To assess health status before beginning strenuous physical activity programmes

### Monitoring

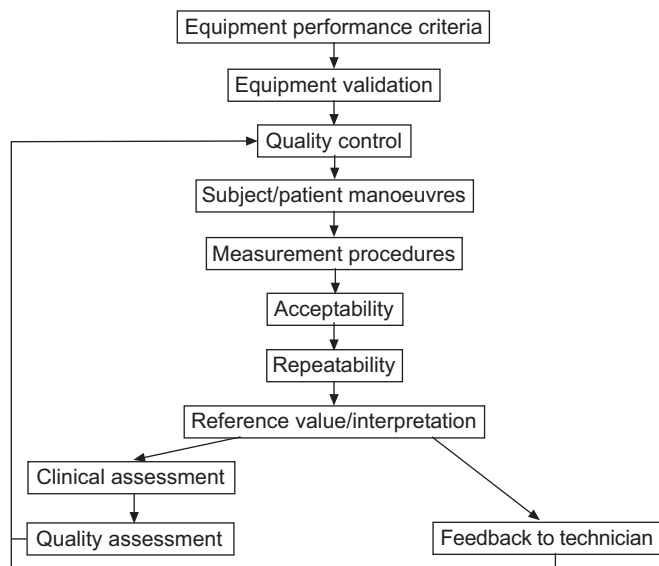
- To assess therapeutic intervention
- To describe the course of diseases that affect lung function
- To monitor people exposed to injurious agents
- To monitor for adverse reactions to drugs with known pulmonary toxicity

### Disability/impairment evaluations

- To assess patients as part of a rehabilitation programme
- To assess risks as part of an insurance evaluation
- To assess individuals for legal reasons

### Public health

- Epidemiological surveys
- Derivation of reference equations
- Clinical research



**FIGURE 1.** Spirometry standardisation steps.

widely. The statement is structured to cover definitions, equipment and patient-related procedures. All recording devices covered by this statement must meet the relevant requirements, regardless of whether they are for monitoring or diagnostic purposes. There is no separate category for “monitoring” devices.

Although manufacturers have the responsibility for producing pulmonary function testing systems that satisfy all the recommendations presented here, it is possible that, for some equipment, meeting all of them may not always be achievable. In these circumstances, manufacturers should clearly identify which equipment requirements have not been met. While manufacturers are responsible for demonstrating the accuracy and reliability of the systems that they sell, it is the user who is responsible for ensuring that the equipment’s measurements remain accurate. The user is also responsible for following local law, which may have additional requirements. Finally, these guidelines are minimum guidelines, which may not be sufficient for all settings, such as when conducting research, epidemiological studies, longitudinal evaluations and occupational surveillance.

## FEV<sub>1</sub> AND FVC MANOEUVRE

### Definitions

FVC is the maximal volume of air exhaled with maximally forced effort from a maximal inspiration, *i.e.* vital capacity performed with a maximally forced expiratory effort, expressed in litres at body temperature and ambient pressure saturated with water vapour (BTPS; see *BTPS correction* section).

FEV<sub>1</sub> is the maximal volume of air exhaled in the first second of a forced expiration from a position of full inspiration, expressed in litres at BTPS.

### Equipment

#### Requirements

The spirometer must be capable of accumulating volume for  $\geq 15$  s (longer times are recommended) and measuring

volumes of  $\geq 8$  L (BTPS) with an accuracy of at least  $\pm 3\%$  of reading or  $\pm 0.050$  L, whichever is greater, with flows between 0 and  $14$  L·s<sup>-1</sup>. The total resistance to airflow at  $14.0$  L·s<sup>-1</sup> must be  $< 1.5$  cmH<sub>2</sub>O·L<sup>-1</sup>·s<sup>-1</sup> ( $0.15$  kPa·L<sup>-1</sup>·s<sup>-1</sup>; see *Minimal recommendations for spirometry systems* section). The total resistance must be measured with any tubing, valves, pre-filter, *etc.* included that may be inserted between the subject and the spirometer. Some devices may exhibit changes in resistance due to water vapour condensation, and accuracy requirements must be met under BTPS conditions for up to eight successive FVC manoeuvres performed in a 10-min period without inspiration from the instrument.

### Display

For optimal quality control, both flow–volume and volume–time displays are useful, and test operators should visually inspect the performance of each manoeuvre for quality assurance before proceeding with another manoeuvre. This inspection requires tracings to meet the minimum size and resolution requirements set forth in this standard.

Displays of flow *versus* volume provide more detail for the initial portion (first 1 s) of the FVC manoeuvre. Since this portion of the manoeuvre, particularly the peak expiratory flow (PEF), is correlated with the pleural pressure during the manoeuvre, the flow–volume display is useful to assess the magnitude of effort during the initial portions of the manoeuvre. The ability to overlay a series of flow–volume curves registered at the point of maximal inhalation may be helpful in evaluating repeatability and detecting sub-maximal efforts. However, if the point of maximal inhalation varies between blows, then the interpretation of these results is difficult because the flows at identical measured volumes are being achieved at different absolute lung volumes. In contrast, display of the FVC manoeuvre as a volume–time graph provides more detail for the latter part of the manoeuvre. A volume–time tracing of sufficient size also allows independent measurement and calculation of parameters from the FVC manoeuvres. In a display of multiple trials, the sequencing of the blows should be apparent to the user.

For the start of test display, the volume–time display should include  $\geq 0.25$  s, and preferably 1 s, before exhalation starts (zero volume). This time period before there is any change in volume is needed to calculate the back extrapolated volume (EV; see *Start of test criteria* section) and to evaluate effort during the initial portion of the manoeuvre. Time zero, as defined by EV, must be presented as the zero point on the graphical output.

The last 2 s of the manoeuvre should be displayed to indicate a satisfactory end of test (see *End of test criteria* section).

When a volume–time curve is plotted as hardcopy, the volume scale must be  $\geq 10$  mm·L<sup>-1</sup> (BTPS). For a screen display, 5 mm·L<sup>-1</sup> is satisfactory (table 2).

The time scale should be  $\geq 20$  mm·s<sup>-1</sup>, and larger time scales are preferred ( $\geq 30$  mm·s<sup>-1</sup>) when manual measurements are made [1, 6, 7]. When the volume–time plot is used in conjunction with a flow–volume curve (*i.e.* both display methods are provided for interpretations and no hand

**TABLE 2** Recommended minimum scale factors for time, volume and flow on graphical output

Parameter	Instrument display		Hardcopy graphical output	
	Resolution required	Scale factor	Resolution required	Scale factor
Volume <sup>#</sup>	0.050 L	5 mm·L <sup>-1</sup>	0.025 L	10 mm·L <sup>-1</sup>
Flow <sup>#</sup>	0.200 L·s <sup>-1</sup>	2.5 mm·L <sup>-1</sup> ·s <sup>-1</sup>	0.100 L·s <sup>-1</sup>	5 mm·L <sup>-1</sup> ·s <sup>-1</sup>
Time	0.2 s	10 mm·s <sup>-1</sup>	0.2 s	20 mm·s <sup>-1</sup>

<sup>#</sup>: the correct aspect ratio for a flow versus volume display is two units of flow per one unit of volume.

measurements are performed), the time scale requirement is reduced to 10 mm·s<sup>-1</sup> from the usually required minimum of 20 mm·s<sup>-1</sup> (table 2). The rationale for this exception is that the flow–volume curve can provide the means for quality assessment during the initial portion of the FVC manoeuvre. The volume–time curve can be used to evaluate the latter part of the FVC manoeuvre, making the time scale less critical.

#### Validation

It is strongly recommended that spirometry systems should be evaluated using a computer-driven mechanical syringe or its equivalent, in order to test the range of exhalations that are likely to be encountered in the test population. Testing the performance of equipment is not part of the usual laboratory procedures (see *Test signals for spirometer testing* section).

#### Quality control

Attention to equipment quality control and calibration is an important part of good laboratory practice. At a minimum, the requirements are as follows: 1) a log of calibration results is maintained; 2) the documentation of repairs or other alterations which return the equipment to acceptable operation; 3) the dates of computer software and hardware updates or changes; and 4) if equipment is changed or relocated (e.g. industrial surveys), calibration checks and quality-control procedures must be repeated before further testing begins.

Key aspects of equipment quality control are summarised in table 3.

Calibration is the procedure for establishing the relationship between sensor-determined values of flow or volume and the actual flow or volume.

A calibration check is different from calibration and is the procedure used to validate that the device is within calibration limits, e.g.  $\pm 3\%$  of true. If a device fails its calibration check, then a new calibration procedure or equipment maintenance is required. Calibration checks must be undertaken daily, or more frequently, if specified by the manufacturer.

The syringe used to check the volume calibration of spirometers must have an accuracy of  $\pm 15$  mL or  $\pm 0.5\%$  of the full scale (15 mL for a 3-L syringe), and the manufacturer must

**TABLE 3** Summary of equipment quality control

Test	Minimum interval	Action
Volume	Daily	Calibration check with a 3-L syringe
Leak	Daily	3 cmH <sub>2</sub> O (0.3 kPa) constant pressure for 1 min
Volume linearity	Quarterly	1-L increments with a calibrating syringe measured over entire volume range
Flow linearity	Weekly	Test at least three different flow ranges
Time	Quarterly	Mechanical recorder check with stopwatch
Software	New versions	Log installation date and perform test using "known" subject

provide recommendations concerning appropriate intervals between syringe calibration checks. Users should be aware that a syringe with an adjustable or variable stop may be out of calibration if the stop is reset or accidentally moved. Calibration syringes should be periodically (e.g. monthly) leak tested at more than one volume up to their maximum; this can be done by attempting to empty them with the outlet corked. A dropped or damaged syringe should be considered out of calibration until it is checked.

With regard to time, assessing mechanical recorder time scale accuracy with a stopwatch must be performed at least quarterly. An accuracy of within 2% must be achieved.

#### Quality control for volume-measuring devices

The volume accuracy of the spirometer must be checked at least daily, with a single discharge of a 3-L calibrated syringe. Daily calibration checking is highly recommended so that the onset of a problem can be determined within 1 day, and also to help define day-to-day laboratory variability. More frequent checks may be required in special circumstances, such as: 1) during industrial surveys or other studies in which a large number of subject manoeuvres are carried out, the equipment's calibration should be checked more frequently than daily [8]; and 2) when the ambient temperature is changing (e.g. field studies), volume accuracy must be checked more frequently than daily and the BTPS correction factor appropriately updated.

The accuracy of the syringe volume must be considered in determining whether the measured volume is within acceptable limits. For example, if the syringe has an accuracy of 0.5%, a reading of  $\pm 3.5\%$  is appropriate.

The calibration syringe should be stored and used in such a way as to maintain the same temperature and humidity of the testing site. This is best accomplished by keeping the syringe in close proximity to the spirometer, but out of direct sunlight and away from heat sources.

Volume-type spirometer systems must be evaluated for leaks every day [9, 10]. The importance of undertaking this daily test cannot be overstressed. Leaks can be detected by applying a constant positive pressure of  $\geq 3.0$  cmH<sub>2</sub>O (0.3 kPa) with the spirometer outlet occluded (preferably at or including the mouthpiece). Any observed volume loss  $>30$  mL after 1 min indicates a leak [9, 10] and needs to be corrected.

At least quarterly, volume spirometers must have their calibration checked over their entire volume range using a calibrated syringe [11] or an equivalent volume standard. The measured volume should be within  $\pm 3.5\%$  of the reading or 65 mL, whichever is greater. This limit includes the 0.5% accuracy limit for a 3-L syringe. The linearity check procedure provided by the manufacturer can be used if it is equivalent to one of the following procedures: 1) consecutive injections of 1-L volume increments while comparing observed volume with the corresponding cumulative measured volume, e.g. 0–1, 1–2, 2–3, ... 6–7 and 7–8 L, for an 8-L spirometer; and 2) injection of a 3-L volume starting at a minimal spirometer volume, then repeating this with a 1-L increment in the start position, e.g. 0–3, 1–4, 2–5, 3–6, 4–7 and 5–8 L, for an 8-L spirometer.

The linearity check is considered acceptable if the spirometer meets the volume accuracy requirements for all volumes tested.

#### Quality control for flow-measuring devices

With regards to volume accuracy, calibration checks must be undertaken at least daily, using a 3-L syringe discharged at least three times to give a range of flows varying between 0.5 and 12 L·s<sup>-1</sup> (with 3-L injection times of ~6 s and <0.5 s). The volume at each flow should meet the accuracy requirement of  $\pm 3.5\%$ . For devices using disposable flow sensors, a new sensor from the supply used for patient tests should be tested each day.

For linearity, a volume calibration check should be performed weekly with a 3-L syringe to deliver three relatively constant flows at a low flow, then three at a mid-range flow and finally three at a high flow. The volumes achieved at each of these flows should each meet the accuracy requirement of  $\pm 3.5\%$ .

#### Test procedure

There are three distinct phases to the FVC manoeuvre, as follows: 1) maximal inspiration; 2) a ‘blast’ of exhalation; and 3) continued complete exhalation to the end of test (EOT).

The technician should demonstrate the appropriate technique and follow the procedure described in table 4. The subject should inhale rapidly and completely from functional residual capacity (FRC), the breathing tube should be inserted into the subject’s mouth (if this has not already been done), making sure the lips are sealed around the mouthpiece and that the tongue does not occlude it, and then the FVC manoeuvre should be begun with minimal hesitation. Reductions in PEF and FEV<sub>1</sub> have been shown when inspiration is slow and/or there is a 4–6 s pause at total lung capacity (TLC) before beginning exhalation [12]. It is, therefore, important that the preceding inspiration is fast and any pause at full inspiration be minimal (*i.e.* only for 1–2 s). The test assumes a full inhalation before beginning the forced exhalation, and it is imperative that the subject takes a complete inhalation before beginning the manoeuvre. The subject should be prompted to ‘blast,’ not just ‘blow,’ the air from their lungs, and then he/she should be encouraged to fully exhale. Throughout the manoeuvre, enthusiastic coaching of the subject using appropriate body language and phrases, such as ‘keep going’, is

**TABLE 4** Procedures for recording forced vital capacity

#### Check the spirometer calibration

#### Explain the test

#### Prepare the subject

- Ask about smoking, recent illness, medication use, etc.
- Measure weight and height without shoes

#### Wash hands

#### Instruct and demonstrate the test to the subject, to include

- Correct posture with head slightly elevated
- Inhale rapidly and completely
- Position of the mouthpiece (open circuit)
- Exhale with maximal force

#### Perform manoeuvre (closed circuit method)

- Have subject assume the correct posture
- Attach nose clip, place mouthpiece in mouth and close lips around the mouthpiece
- Inhale completely and rapidly with a pause of <1 s at TLC
- Exhale maximally until no more air can be expelled while maintaining an upright posture
- Repeat instructions as necessary, coaching vigorously
- Repeat for a minimum of three manoeuvres; no more than eight are usually required
- Check test repeatability and perform more manoeuvres as necessary

#### Perform manoeuvre (open circuit method)

- Have subject assume the correct posture
- Attach nose clip
- Inhale completely and rapidly with a pause of <1 s at TLC
- Place mouthpiece in mouth and close lips around the mouthpiece
- Exhale maximally until no more air can be expelled while maintaining an upright posture
- Repeat instructions as necessary, coaching vigorously
- Repeat for a minimum of three manoeuvres; no more than eight are usually required
- Check test repeatability and perform more manoeuvres as necessary

TLC: total lung capacity.

required. It is particularly helpful to observe the subject with occasional glances to check for distress, and to observe the tracing or computer display during the test to help ensure maximal effort. If the patient feels ‘dizzy’, the manoeuvre should be stopped, since syncope could follow due to prolonged interruption of venous return to the thorax. This is more likely to occur in older subjects and those with airflow limitation. Performing a vital capacity (VC) manoeuvre (see *VC and IC manoeuvre* section), instead of obtaining FVC, may help to avoid syncope in some subjects. Reducing the effort part-way through the manoeuvre [13] may give a higher expiratory volume in some subjects, but then is no longer a maximally forced expiration. Well-fitting false teeth should not be routinely removed, since they preserve oropharyngeal geometry and spirometry results are generally better with them in place [14].

With appropriate coaching, children as young as 5 yrs of age are often able to perform acceptable spirometry [15]. The technicians who are involved in the pulmonary function testing of children should be specifically trained to deal with such a situation. A bright, pleasant atmosphere,

including age-appropriate toys, reading material and art, is important in making children feel at ease. Encouragement, detailed but simple instructions, lack of intimidation and visual feedback in the teaching are important in helping children to perform the manoeuvre. Even if unsuccessful at the first session, children will learn to be less intimidated and may perform far better in a subsequent session. Testing children in "adult" laboratories, where no effort is made to cater for the specific needs of the younger subjects, is to be discouraged.

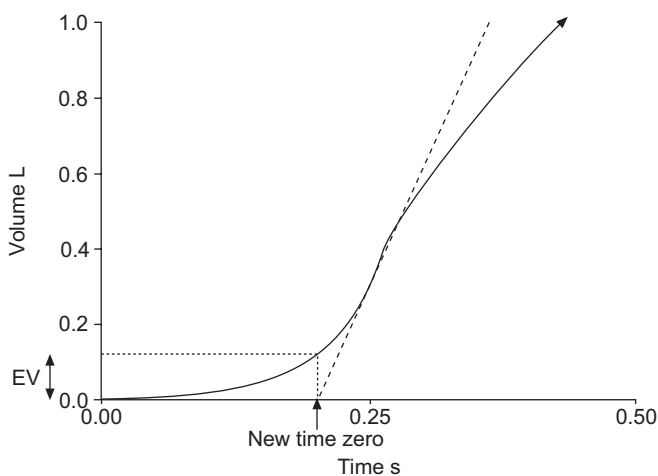
The use of a nose clip or manual occlusion of the nares is recommended, and, for safety reasons, testing should be preferably done in the sitting position, using a chair with arms and without wheels. If testing is undertaken with the patient standing or in another position, this must be documented on the report.

### Within-manoeuve evaluation

#### Start of test criteria

The start of test, for the purpose of timing, is determined by the back extrapolation method (fig. 2) [1, 3, 9, 16]. The new "time zero" from back extrapolation defines the start for all timed measurements. For manual measurements, the back extrapolation method traces back from the steepest slope on the volume-time curve [17]. For computerised back extrapolation, it is recommended that the largest slope averaged over an 80-ms period is used [18]. Figure 2 provides an example and explanation of back extrapolation and the derivation of EV. To achieve an accurate time zero and assure the FEV<sub>1</sub> comes from a maximal effort curve, the EV must be <5% of the FVC or 0.150 L, whichever is greater. If a manoeuvre has an obviously hesitant start, the technician may terminate the trial early to avoid an unnecessary prolonged effort.

Rapid computerised feedback to the technician when the start criteria are not met is strongly encouraged. In addition to the expiratory manoeuvre, the volume-time curve display (graph)



**FIGURE 2.** Expanded version of the early part of a subject's volume-time spirogram, illustrating back extrapolation through the steepest part of the curve, where flow is peak expiratory flow (PEF), to determine the new "time zero". Forced vital capacity (FVC)=4.291 L; back extrapolated volume (EV)=0.123 L (2.9% FVC). -----: back extrapolation line through PEF.

should ideally include the whole preceding inspiratory manoeuvre, but must include  $\geq 0.25$  s and preferably  $\geq 1$  s prior to the start of exhalation (time zero). The equipment should display the EV value. Inspection of the flow-volume curve may be added as a measure of the satisfactory start of test. PEF should be achieved with a sharp rise and occur close to the point of maximal inflation, *i.e.* the start of exhalation (see *Equipment* section).

#### End of test criteria

It is important for subjects to be verbally encouraged to continue to exhale the air at the end of the manoeuvre to obtain optimal effort, *e.g.* by saying "keep going". EOT criteria are used to identify a reasonable FVC effort, and there are two recommended EOT criteria, as follows. 1) The subject cannot or should not continue further exhalation. Although subjects should be encouraged to achieve their maximal effort, they should be allowed to terminate the manoeuvre on their own at any time, especially if they are experiencing discomfort. The technician should also be alert to any indication that the patient is experiencing discomfort, and should terminate the test if a patient is becoming uncomfortable or is approaching syncope. 2) The volume-time curve shows no change in volume (<0.025 L) for  $\geq 1$  s, and the subject has tried to exhale for  $\geq 3$  s in children aged <10 yrs and for  $\geq 6$  s in subjects aged >10 yrs.

The equipment should signal to the technician if the plateau criteria were not met. A satisfactory EOT may still have been achieved, but an equipment alert will help the technician to pinpoint where the subject may need more encouragement. It is of note that a closure of the glottis may prematurely terminate a manoeuvre at <6 s, even when the apparent duration of the blow exceeds 6 s.

For patients with airways obstruction or older subjects, exhalation times of >6 s are frequently needed. However, exhalation times of >15 s will rarely change clinical decisions. Multiple prolonged exhalations are seldom justified and may cause light headedness, syncope, undue fatigue and unnecessary discomfort.

Achieving EOT criteria is one measure of manoeuvre acceptability. Manoeuvres that do not meet EOT criteria should not be used to satisfy the requirement of three acceptable manoeuvres. However, early termination, by itself, is not a reason to eliminate all the results from such a manoeuvre from further consideration. Information such as the FEV<sub>1</sub> may be useful (depending on the length of exhalation) and can be reported from these early terminated manoeuvres.

Some young children may have difficulty meeting the ATS EOT criteria [3], although they may meet other repeatability criteria [19]. Curve-fitting techniques [20] may prove useful in developing new EOT criteria specific for young children.

#### Additional criteria

A cough during the first second of the manoeuvre can affect the measured FEV<sub>1</sub> value. Coughing in the first second or any other cough that, in the technician's judgment, interferes with the measurement of accurate results [3] will render a test unacceptable.

A Valsalva manoeuvre (glottis closure) or hesitation during the manoeuvre that causes a cessation of airflow in a manner that precludes an accurate estimate of either FEV<sub>1</sub> or FVC [3] will render a test unacceptable.

There must be no leak at the mouth [3]. Patients with neuromuscular disease may require manual or other assistance from the technician to guarantee an adequate seal.

Obstruction of the mouthpiece, *e.g.* by the tongue being placed in front of the mouthpiece or by teeth in front of the mouthpiece, or by distortion from biting, may affect the performance of either the device or the subject.

#### Summary of acceptable blow criteria

The acceptability criteria are a satisfactory start of test and a satisfactory EOT, *i.e.* a plateau in the volume–time curve. In addition, the technician should observe that the subject understood the instructions and performed the manoeuvre with a maximum inspiration, a good start, a smooth continuous exhalation and maximal effort. The following conditions must also be met: 1) without an unsatisfactory start of expiration, characterised by excessive hesitation or false start extrapolated volume or EV >5% of FVC or 0.150 L, whichever is greater (fig. 2); 2) without coughing during the first second of the manoeuvre, thereby affecting the measured FEV<sub>1</sub> value, or any other cough that, in the technician's judgment, interferes with the measurement of accurate results [3]; 3) without early termination of expiration (see *End of test criteria* section); 4) without a Valsalva manoeuvre (glottis closure) or hesitation during the manoeuvre that causes a cessation of airflow, which precludes accurate measurement of FEV<sub>1</sub> or FVC [3]; 5) without a leak [3]; 6) without an obstructed mouthpiece (*e.g.* obstruction due to the tongue being placed in front of the mouthpiece, or teeth in front of the mouthpiece, or mouthpiece deformation due to biting); and 7) without evidence of an extra breath being taken during the manoeuvre.

It should be noted that a usable curve must only meet conditions 1 and 2 above, while an acceptable curve must meet all of the above seven conditions.

It is desirable to use a computer-based system that provides feedback to the technician when the above conditions are not met. The reporting format should include qualifiers indicating the acceptability of each manoeuvre. However, failure to meet these goals should not necessarily prevent reporting of results, since, for some subjects, this is their best performance. Records of such manoeuvres should be retained since they may contain useful information.

#### Between-manoevrue evaluation

Using the previously described criteria, an adequate test requires a minimum of three acceptable FVC manoeuvres. Acceptable repeatability is achieved when the difference between the largest and the next largest FVC is  $\leq 0.150$  L and the difference between the largest and next largest FEV<sub>1</sub> is  $\leq 0.150$  L [21]. For those with an FVC of  $\leq 1.0$  L, both these values are 0.100 L. If these criteria are not met in three manoeuvres, additional trials should be attempted, up to, but usually no more than, eight manoeuvres. Large variability among tests is often due to incomplete inhalations. Some patients may require a brief rest period between manoeuvres.

Volume–time or flow–volume curves from at least the best three FVC manoeuvres must be retained. Table 5 gives a summary of the within- and between-manoevrue evaluation.

#### Manoevrue repeatability

For FVC measurements, acceptability must be determined by ascertaining that the recommendations outlined previously on performing the FVC test are met. The guidelines of the ATS [3] contain examples of unacceptable volume–time and corresponding flow–volume curves. Figure 3 shows a flow chart outlining how the criteria for blow acceptability are applied before those for repeatability.

The repeatability criteria are used to determine when more than three acceptable FVC manoeuvres are needed; these criteria are not to be used to exclude results from reports or to exclude subjects from a study. Labelling results as being derived from data that do not conform to the repeatability criteria described previously is recommended. In addition, the repeatability criteria are minimum requirements. Many subjects are able to achieve FVC and FEV<sub>1</sub> repeatability to within 0.150 L. Manoeuvres with an unacceptable start of test or a cough (unusable curve) must be discarded before applying the repeatability criteria and cannot be used in determining the best values. Manoeuvres with early termination or a Valsalva manoeuvre may be used for selecting the largest FVC and FEV<sub>1</sub>.

**TABLE 5** Summary of within- and between-manoevrue acceptability criteria

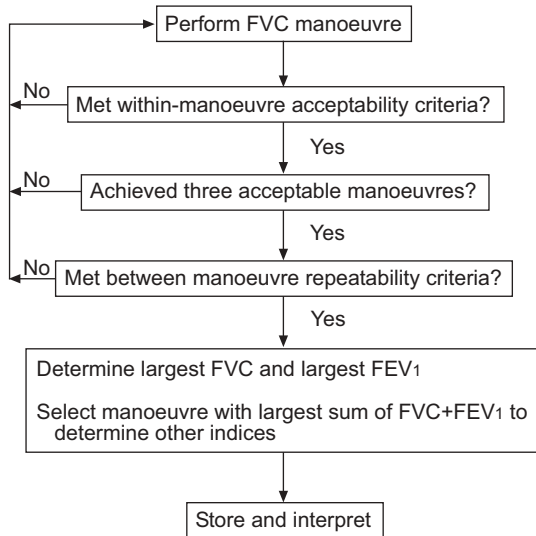
#### Within-manoevrue criteria

- Individual spiromgrams are "acceptable" if
  - They are free from artefacts [3]
    - Cough during the first second of exhalation
    - Glottis closure that influences the measurement
    - Early termination or cut-off
    - Effort that is not maximal throughout
    - Leak
    - Obstructed mouthpiece
  - They have good starts
    - Extrapolated volume <5% of FVC or 0.15 L, whichever is greater
  - They show satisfactory exhalation
    - Duration of  $\geq 6$  s (3 s for children) or a plateau in the volume–time curve or
      - If the subject cannot or should not continue to exhale

#### Between-manoevrue criteria

- After three acceptable spiromgrams have been obtained, apply the following tests
  - The two largest values of FVC must be within 0.150 L of each other
  - The two largest values of FEV<sub>1</sub> must be within 0.150 L of each other
- If both of these criteria are met, the test session may be concluded
- If both of these criteria are not met, continue testing until
  - Both of the criteria are met with analysis of additional acceptable spiromgrams or
  - A total of eight tests have been performed (optional) or
  - The patient/subject cannot or should not continue
- Save, as a minimum, the three satisfactory manoeuvres

FVC: forced vital capacity; FEV<sub>1</sub>: forced expiratory volume in one second.



**FIGURE 3.** Flow chart outlining how acceptability and repeatability criteria are to be applied. FVC: forced vital capacity; FEV<sub>1</sub>: forced expiratory volume in one second.

No spirogram or test result should be rejected solely on the basis of its poor repeatability. The repeatability of results should be considered at the time of interpretation. The use of data from manoeuvres with poor repeatability or failure to meet the EOT requirements is left to the discretion of the interpreter.

#### Maximum number of manoeuvres

Although there may be some circumstances in which more than eight consecutive FVC manoeuvres may be needed, eight is generally a practical upper limit for most subjects [22, 23]. After several forced expiratory manoeuvres, fatigue can begin to take its toll on subjects and additional manoeuvres would be of little added value. In extremely rare circumstances, subjects may show a progressive reduction in FEV<sub>1</sub> or FVC with each subsequent blow. If the cumulative drop exceeds 20% of start value, the test procedure should be terminated in the interest of patient safety. The sequence of the manoeuvres should be recorded.

#### Test result selection

FVC and FEV<sub>1</sub> should be measured from a series of at least three forced expiratory curves that have an acceptable start of test and are free from artefact, such as a cough (*i.e.* “usable curves”). The largest FVC and the largest FEV<sub>1</sub> (BTPS) should be recorded after examining the data from all of the usable curves, even if they do not come from the same curve.

#### Other derived indices

##### FEV<sub>t</sub>

FEV<sub>t</sub> is the maximal volume exhaled by time *t* seconds (timed from the time zero defined by back extrapolation) of a forced expiration from a position of full inspiration, expressed in litres at BTPS. Very young children may not be able to produce prolonged expirations, but there is increasing evidence that indices derived from blows with forced expiratory times of

<1 s may have clinical usefulness [19]. At present, there are insufficient data to recommend the use of FEV<sub>0.5</sub> or FEV<sub>0.75</sub>.

When the subject does not exhale completely, the volume accumulated over a shorter period of time (*e.g.* 6 s) may be used as an approximate surrogate for FVC. When such surrogates are used, the volume label should reflect the shorter exhalation time (*e.g.* FEV<sub>6</sub> for a 6-s exhalation). FEV<sub>6</sub> has been increasingly considered a reasonably reliable surrogate for FVC [24] and can be used for normalising FEV<sub>1</sub> (*e.g.* FEV<sub>1</sub>/FEV<sub>6</sub>). Recording FEV<sub>6</sub> seems to have the advantage of being more reproducible than FVC, being less physically demanding for patients and providing a more explicit EOT. Confirmation from other studies is required.

#### Standardisation of FEV<sub>1</sub> for expired volume, FEV<sub>1</sub>/FVC and FEV<sub>1</sub>/VC

In some patients, a slow or unforced VC or inspiratory vital capacity (IVC) manoeuvre (see *VC and IC manoeuvre* section) may provide a larger and more appropriate denominator for calculation of the FEV<sub>1</sub>/VC%. Some investigators have reported that the VC is slightly higher than the FVC in normal subjects [25].

#### FEF<sub>25–75%</sub>

The mean forced expiratory flow between 25% and 75% of the FVC (FEF<sub>25–75%</sub>) has also been known as the maximum mid-expiratory flow. This index is taken from the blow with the largest sum of FEV<sub>1</sub> and FVC. The FEF<sub>25–75%</sub> must be measured with an accuracy of at least  $\pm 5\%$  of reading or  $\pm 0.200 \text{ L}\cdot\text{s}^{-1}$  whichever is greater, over a range of up to  $7 \text{ L}\cdot\text{s}^{-1}$ . It should be noted that it is highly dependent on the validity of the FVC measurement and the level of expiratory effort.

#### PEF

PEF is usually obtained from flow–volume curve data. It is the maximum expiratory flow achieved from a maximum forced expiration, starting without hesitation from the point of maximal lung inflation, expressed in  $\text{L}\cdot\text{s}^{-1}$ . When PEF is recorded using a patient-administered portable PEF meter, it is often expressed in  $\text{L}\cdot\text{min}^{-1}$ . PEF is covered in more detail later.

#### Maximal expiratory flow–volume loops

The shape of a maximum flow–volume loop (MFVL), which includes forced inspiratory manoeuvres, can be helpful in quality control and in detecting the presence of upper airway obstruction. None of the numerical indices from a MFVL has clinical utility superior to FEV<sub>1</sub>, FVC, FEF<sub>25–75%</sub> and PEF, and are not considered in detail here.

#### Definitions

With regard to instantaneous flows, the recommended measure is the instantaneous forced expiratory flow when X% of the FVC has been expired (FEF<sub>X%</sub>). The maximal instantaneous forced expiratory flow when X% of the FVC remains to be expired (MEF<sub>X%</sub>) was the term previously recommended in Europe.

Instantaneous forced inspiratory flow when X% of the FVC has been expired (FIF<sub>X%</sub>) and mid-inspiratory flow when X% of the FVC has been expired refer to the flows measured on the inspiratory limb of a flow–volume loop. FIF<sub>25–75%</sub>, also



referred to as maximal mid-inspiratory flow, is analogous to FEF<sub>25–75%</sub> (see *Other derived indices* section).

#### Equipment

Instantaneous flows must be measured with an accuracy of  $\pm 5\%$  of reading or  $\pm 0.200 \text{ L}\cdot\text{s}^{-1}$ , whichever is greater, over a range of  $-14$ – $14 \text{ L}\cdot\text{s}^{-1}$ . The level of minimum detectable flow should be  $0.025 \text{ L}\cdot\text{s}^{-1}$ . When a maximum flow–volume loop is plotted or displayed, exhaled flow must be plotted upwards, and exhaled volume towards the right. A 2:1 ratio must be maintained between the flow and volume scales, e.g.  $2 \text{ L}\cdot\text{s}^{-1}$  of flow and 1 L of exhaled volume must be the same distance on their respective axes. The flow and volume scales, used in reviewing test performance, must be equivalent to that shown in table 2.

#### Test procedure

The subject has to make a full expiratory and inspiratory loop as a single manoeuvre. In many laboratories, this is the primary manoeuvre for spirometry. The subject is asked to take a rapid full inspiration to TLC from room air through the mouth, then insert the mouthpiece and, without hesitation, perform an expiration with maximum force until no more gas can be expelled, followed by a quick maximum inspiration. At this point, the manoeuvre is finished.

An alternative procedure is for the subject to insert the mouthpiece while undertaking tidal breathing at FRC, and then, in one continuous sequence, do the following: make a slow expiration to residual volume (RV); followed directly by a slow inspiration to TLC; follow this by a rapid full expiration with maximal effort to RV; and followed by a rapid full inspiration with maximal effort back to TLC.

This procedure is slightly more complicated and may not be suitable for all equipment, but it obtains a measurement of VC as well as FVC.

#### Within- and between-manoevrue evaluation

These evaluations are the same as for FVC (see *Within-manoevrue evaluation* and *Between-manoevrue evaluation* sections). Occasionally, a subject is unable to perform a satisfactory inspiratory limb immediately following a maximal forced expiratory manoeuvre. This is particularly common in the elderly and the infirm. In these circumstances, it may be necessary for the subject to record an inspiratory manoeuvre separately from the expiratory manoeuvre. Equipment should be able to perform these separately and then present three or more loops together on a graphical display or output.

#### Flow–volume loop examples

The following figures (figures 4–10) give typical examples of commonly encountered flow–volume loop configurations. The advantages of visual pattern recognition from the MFVL can readily be appreciated. The shapes of the manoeuvres must be repeatable (fig. 10) for any interpretation to be made. This is especially true for the plateau effect on expiratory and inspiratory limbs of the manoeuvre found in upper airway obstruction, as this can be mimicked by poor effort, which is usually variable from blow to blow. A further explanation is given in the ATS/ERS statement on lung function interpretation [26].

#### Reversibility testing

A determination of airflow-limitation reversibility with drug administration is commonly undertaken as part of lung function testing. The choice of drug, dose and mode of delivery is a clinical decision depending on what the clinician wishes to learn from the test.

If the aim of the test is to determine whether the patient's lung function can be improved with therapy in addition to their regular treatment, then the subject can continue with his/her regular medication prior to the test.

If the clinician wants to determine whether there is any evidence of reversible airflow limitation, then the subject should undergo baseline function testing when not taking any drugs prior to the test. Short-acting inhaled drugs (e.g. the  $\beta$ -agonist albuterol/salbutamol or the anticholinergic agent ipratropium bromide) should not be used within 4 h of testing. Long-acting  $\beta$ -agonist bronchodilators (e.g. salmeterol or formoterol) and oral therapy with aminophylline or slow-release  $\beta$ -agonists should be stopped for 12 h prior to the test. Smoking should be avoided for  $\geq 1$  h prior to testing and throughout the duration of the test procedure.

#### Method

The following steps are undertaken. 1) The subject has three acceptable tests of FEV<sub>1</sub>, FVC and PEF recorded as described previously. 2) The drug is administered in the dose and by the method indicated for the test. For example, after a gentle and incomplete expiration, a dose of 100  $\mu\text{g}$  of albuterol/salbutamol is inhaled in one breath to TLC from a valved spacer device. The breath is then held for 5–10 s before the subject exhales. Four separate doses (total dose 400  $\mu\text{g}$ ) are delivered at  $\sim 30$ -s intervals. This dose ensures that the response is high on the albuterol dose–response curve. A lower dose can be used if there is concern about any effect on the patient's heart rate or tremor. Other drugs can also be used. For the anticholinergic agent ipratropium bromide, the total dose is 160  $\mu\text{g}$  ( $4 \times 40 \mu\text{g}$ ).

Three additional acceptable tests are recorded  $\geq 10$  min and up to 15 min later for short-acting  $\beta$ -agonists, and 30 min later for short-acting anticholinergic agents.

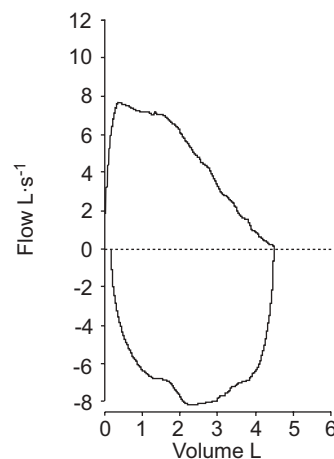
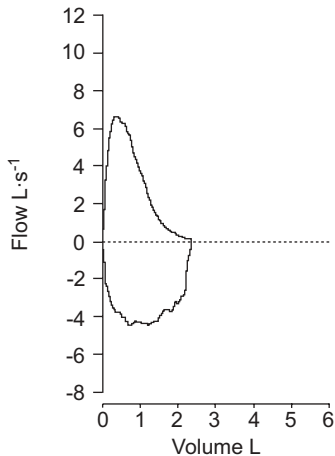
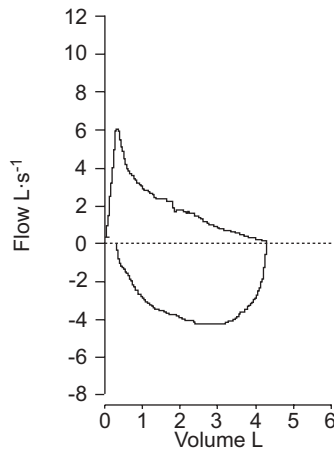


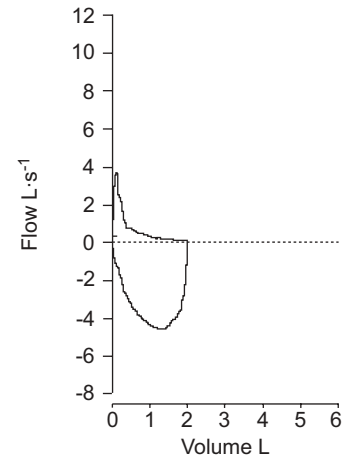
FIGURE 4. Flow–volume loop of a normal subject.



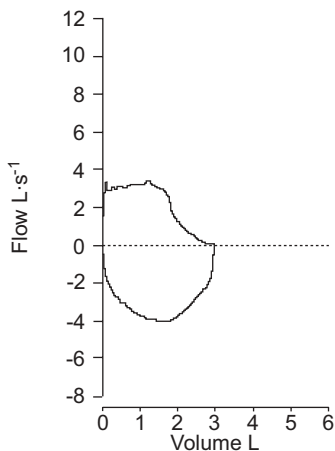
**FIGURE 5.** Flow-volume loop of a normal subject with end expiratory curvilinearity, which can be seen with ageing.



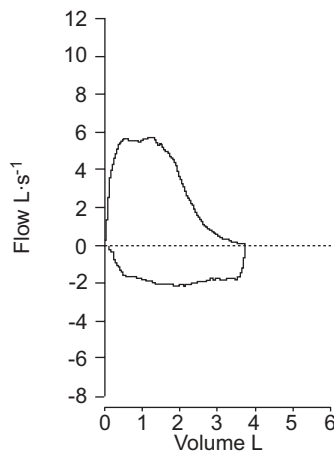
**FIGURE 6.** Moderate airflow limitation in a subject with asthma.



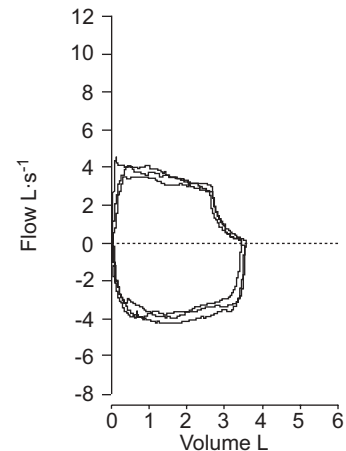
**FIGURE 7.** Severe airflow limitation in a subject with chronic obstructive pulmonary disease.



**FIGURE 8.** Variable intra-thoracic upper airway obstruction.



**FIGURE 9.** Variable extra-thoracic upper airway obstruction.



**FIGURE 10.** Fixed upper airway obstruction shown by three manoeuvres.

Comment on dose and delivery method

Standardising the bronchodilator dose administered is necessary in order to standardise the definition of a significant bronchodilator response. The rate of pulmonary deposition of a drug with tidal breathing from an unvented nebuliser will depend on drug concentration, rate of nebuliser output, particle-size distribution, and the ratio of the time spent in inspiration over the total respiratory time ( $t_i/t_{tot}$ ) [27]. The fraction of the aerosol carried in particles with a diameter of  $\leq 5 \mu\text{m}$  that is expected to deposit in adult lungs if inhaled through a mouthpiece [28] is defined as the respirable fraction (RF). For example, 2.5 mg of salbutamol (albuterol) in 2.5 mL of solution, placed in a Hudson Updraft II (Hudson RCI, Temecula, CA, USA) driven by a PulmoAide compressor (De Vilbiss, Somerset, PA, USA), would produce  $\sim 0.1 \text{ mg} \cdot \text{min}^{-1}$  in the RF. For a respiratory rate of  $15 \text{ breaths} \cdot \text{min}^{-1}$  and a  $t_i/t_{tot}$  of 0.45, this would give  $\sim 3 \mu\text{g}$  deposited in the lungs per breath, or  $45 \mu\text{g} \cdot \text{min}^{-1}$ . For adults using a metered dose

inhaler (MDI) with a valve-holding chamber (spacer), between 10 and 20% [29, 30] of a  $100\text{-}\mu\text{g}$  "puff" (or  $\sim 15 \mu\text{g}$  per activation) would be expected to be deposited in the lung of an adult. Without a spacer, the deposition will be less, and heavily technique dependent [31]. Pulmonary deposition from dry-powder inhalers is device specific, and breath-enhanced nebulisers deposit much more than unvented ones [32, 33]. CFC-free MDIs produce a smaller particle-size distribution and improved (up to 50% of dose) lung deposition compared with those with CFC propellant [34]. For children, pulmonary deposition is less than that in adults [35], possibly relating to the size of the upper airway. Each laboratory should be familiar with the pulmonary-deposition characteristics of the devices they use.

Determination of reversibility

This aspect is covered in detail in the interpretative strategy document of the ATS and ERS [26].

## VC AND IC MANOEUVRE

### Definitions

#### VC and IVC

The VC is the volume change at the mouth between the position of full inspiration and complete expiration, expressed in litres at BTPS. The slow VC can be derived in two ways. The expiratory vital capacity (EVC) is the maximal volume of air exhaled from the point of maximal inhalation. The IVC is the maximal volume of air inhaled from the point of maximal exhalation, achieved by a slow expiration from end-tidal inspiration. These manoeuvres are unforced, except at the point of reaching RV or TLC, respectively, where extra effort is required [36].

#### IC

Inspiratory capacity (IC) is volume change recorded at the mouth when taking a slow full inspiration with no hesitation, from a position of passive end-tidal expiration, *i.e.* FRC, to a position of maximum inspiration, expressed in litres at BTPS. IC is an indirect estimate of the degree of lung hyperinflation at rest, and is useful to assess changes in FRC with pharmacological interventions and physical exercise [37–41].

### Equipment

For measurements of VC and IC, the spirometer or flow meter must comply with the requirements for FVC (as described previously) and be capable of accumulating volume for  $\geq 30$  s.

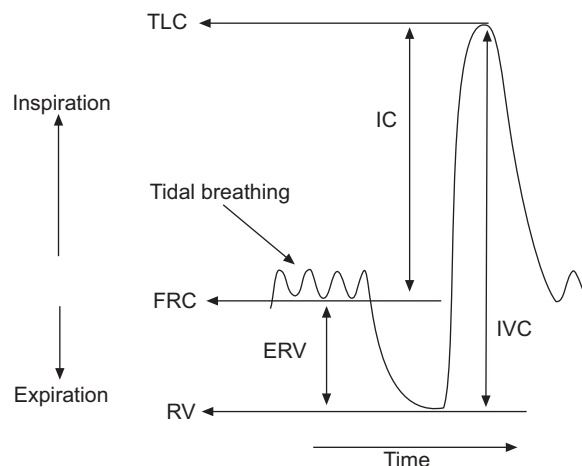
Expiratory manoeuvres or, ideally, both inspiratory and expiratory manoeuvres should be included in the display of VC manoeuvre. Regardless of whether the inspiratory or expiratory manoeuvre is used for deriving measurements, a display of the entire recorded VC manoeuvre must be provided. The maximal expiratory volume must be assessed to determine whether the subject has obtained a plateau in the expiratory effort. For display of the slow VC, the time scale may be reduced to  $5 \text{ mm}\cdot\text{s}^{-1}$ .

### Test procedure

#### VC

VC can be measured using conventional spirometers. It may also be recorded from equipment used to measure static lung volumes and their subdivisions [42]. For slow VC, a maximum of four manoeuvres is a practical upper limit. It is preferable that VC manoeuvres be performed before FVC manoeuvres because of the potential for muscular fatigue and volume history effects, where, after maximal inspiratory efforts, some patients with severe airways obstruction return to a falsely high level of FRC or RV, due to gas trapping or stress relaxation [3]. The VC manoeuvre may be considered either as an IVC, where the subject inhales completely from a position of full expiration, or as an EVC, where the subject exhales completely from a position of full inspiration. Figure 11 shows the recording of IVC and figure 12 shows an EVC recording. Important differences between inspiratory (*i.e.* IVC) and expiratory (*i.e.* EVC) manoeuvres may be observed in patients with airways obstruction [43, 44].

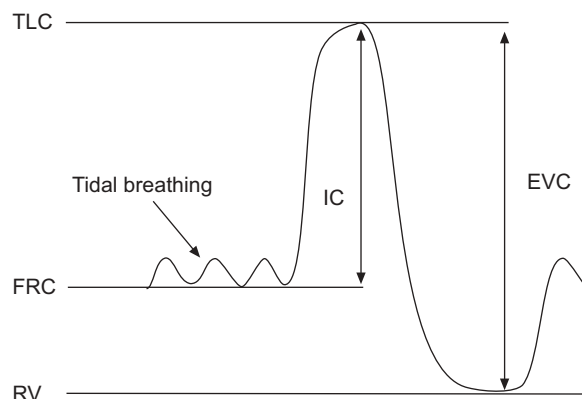
The test is begun by instructing the subject in the VC manoeuvre and demonstrating the appropriate technique. It is important that subjects understand they must completely fill and empty their lungs. The VC manoeuvre is performed with the subject using a mouthpiece and wearing a nose clip. The



**FIGURE 11.** Tracing of tidal breathing followed by an expiratory manoeuvre to residual volume (RV), followed by a full inspiration to total lung capacity (TLC) to record inspiratory vital capacity (IVC) and inspiratory capacity (IC). FRC: functional residual capacity; ERV: expiratory reserve volume.

manoeuvre is not forced; it is performed in a relaxed manner, except near end-inspiration and end-expiration. The subject exhales completely to RV, then inhales to TLC, and finally exhales to RV again. The technician should encourage the subject to reach maximal inhaled and exhaled volumes with a relatively constant flow. The exhalation should not be unduly slow, as this can lead to underestimation of VC. Technicians should observe the subject carefully to ensure that his/her lips are sealed, nothing obstructs the mouthpiece, no leaks occur, and that TLC and RV are reached.

Alternatively, the subject inhales maximally, inserts the mouthpiece just past his/her front teeth, seals his/her lips around the mouthpiece, and blows slowly and evenly until there is no volume change ( $<0.025$  L) for a 1-s period (see *End of test criteria* section). Patients with neuromuscular disease may need assistance in maintaining a tight seal at the mouth. The technician must observe the subject's inhalation to ensure



**FIGURE 12.** Tracing of tidal breathing followed by an inspiratory manoeuvre to total lung capacity (TLC) to record inspiratory capacity (IC), followed by a full expiration to residual volume (RV) to record expiratory reserve volume (EVC). FRC: functional residual capacity.

that it is complete, and that air is not exhaled while the mouthpiece is being inserted. The technician should assure that the expiratory manoeuvre is not forced. In healthy subjects, adequate maximal inspiratory and expiratory levels are achieved within 5–6 s.

#### IC

Subjects should be tested in the seated position wearing a nose clip with no air leaks between the mouth and the mouthpiece. Subjects should be relaxed (shoulders down and relaxed) and asked to breathe regularly for several breaths until the end-expiratory lung volume is stable (this usually requires at least three tidal manoeuvres). They are then urged to take a deep breath to TLC with no hesitation. Figure 12 shows a tracing from the recording of IC.

#### Use of a nose clip

The use of a nose clip is encouraged in VC measurements, since some people breathe through the nose when performing a slow VC manoeuvre. A nose clip must be used when performing inspiratory manoeuvres such as the IVC or IC.

#### Within-manoeuve evaluation

These are the same as for FVC EOT criteria as described previously. There must be no leak at the mouth, no hesitation during the manoeuvre, and no obstruction of the mouthpiece (see *Additional criteria* section). The IC may be underestimated if the inspiratory manoeuvre is too slow due to poor effort or hesitation, or if there is premature closure of the glottis.

#### Between-manoeuve evaluation

As with spirometry, a minimum of three acceptable VC manoeuvres must be obtained. If the difference in VC between the largest and next largest manoeuvre is  $>0.150$  L, additional trials should be undertaken. Meeting repeatability criteria may require that up to, but usually no more than, four manoeuvres are performed, with a rest period of  $\geq 1$  min between the manoeuvres. Large variability in this test is often due to incomplete inhalations. Volume–time curves from the best two VC manoeuvres must be retained. For the IC, at least three acceptable manoeuvres should be performed. The mean coefficient of variation for IC in chronic airflow obstruction has been found to be  $5 \pm 3\%$  [39].

#### Test result selection

For VC, the largest value from at least three acceptable manoeuvres should be reported. For IC, the average of at least three manoeuvres should be reported.

#### PEAK EXPIRATORY FLOW

Studies on the measurement of PEF are ongoing. Recent evidence has suggested that the previously applied standards may allow incorrect measurements to be made [45], and it is possible that more stringent requirements may be required. A further statement will be made when the position on the clinical significance of this is clear. However, since PEF measurements are part of asthma-management programmes, the previous recommendations [3, 46] are reiterated here.

Other instantaneous flow measurements (e.g. FEF<sub>50%</sub>, FEF<sub>75%</sub>) are not proven to be superior to conventional spirometric

indices in a clinical setting, and, therefore, are not considered further.

#### Definition

PEF is the highest flow achieved from a maximum forced expiratory manoeuvre started without hesitation from a position of maximal lung inflation [46]. When it is obtained from flow–volume curve data, it is expressed at BTPS in  $L \cdot s^{-1}$ . The defining characteristics of the flow–time curve, in relation to PEF, are the time taken for flow to rise from 10% of PEF to 90% of PEF, i.e. the rise time (RT), and the duration that flow is  $>90\%$  of PEF, called the dwell time (DT). When PEF is obtained with portable monitoring instruments, it is expressed in  $L \cdot \text{min}^{-1}$ .

#### Equipment

Ideally, PEF should be recorded by an instrument that primarily records flow. Measuring PEF requires an instrument that has a flat frequency response ( $\pm 5\%$ ) up to 15 Hz [46]. Although there is evidence of significant frequency content in PEF up to 20 Hz [47], it is recommended, at this stage, that manufacturers achieve a goal of recording fidelity up to 15 Hz. The PEF must be measured with an accuracy of  $\pm 10\%$  or  $\pm 0.3 L \cdot s^{-1}$  ( $20 L \cdot \text{min}^{-1}$ ), whichever is the greater. Mean instrument resistance measured across the range of the instrument should be  $<2.5 \text{ cmH}_2\text{O} \cdot L^{-1} \cdot s^{-1}$  ( $0.25 \text{ kPa} \cdot L^{-1} \cdot s^{-1}$ ; table 6). PEF is sensitive to the resistance of the meter; for example, a resistance of  $0.25 \text{ kPa} \cdot L^{-1} \cdot s^{-1}$  decreases PEF by  $\sim 8\%$  compared with PEF measured with a low-resistance pneumotachograph [48].

Intra-instrument repeatability must be  $<5\%$  or  $0.150 L \cdot s^{-1}$  ( $10 L \cdot \text{min}^{-1}$ ), whichever is the greater. Inter-device reproducibility must be  $<10\%$  or  $0.300 L \cdot s^{-1}$  ( $20 L \cdot \text{min}^{-1}$ ), whichever is the greater. Calculating PEF by differentiating volume–time data may introduce noise; hence, a parabolic-fitting algorithm may be used [2] as a smoothing procedure.

Equipment validation is covered in the *Test signals for PEF meter testing* section.

#### Test procedure

PEF is dependent on effort and lung volume, with subject cooperation being essential. PEF must be achieved as rapidly as possible and at as high a lung volume as possible, in order to obtain the maximum value [49]. The subject must be encouraged to blow as vigorously as possible. The neck should be in a neutral position, not flexed or extended, and the subject must not cough. A nose clip is not necessary.

After the point of full lung inflation, the subject must deliver the blow without any delay. Hesitating for as little as 2 s or flexing the neck allows the tracheal visco-elastic properties to relax and PEF to drop by as much as 10% [50]. Tonguing, spitting or coughing at the start of the blow may falsely raise the recorded PEF in some devices.

In the laboratory, the subject must perform a minimum of three PEF manoeuvres. When PEF is a self-administered recording, it is important that the subject has been adequately taught how to perform the test, when to perform it and what action to take depending on the resulting value obtained. Regular checks of the patient's PEF technique and meter are an important part of the follow-up.

**Within-manoeuve evaluation**

The subject must be observed to ensure a good seal at the mouth, no hesitation occurred, and there was no abnormal start to the manoeuvre.

**Between-manoeuve evaluation**

The PEF values and their order must be recorded so that manoeuvre-induced bronchospasm can be detected. If the largest two out of three acceptable blows are not reproducible within  $0.67 \text{ L}\cdot\text{s}^{-1}$  ( $40 \text{ L}\cdot\text{min}^{-1}$ ), up to two additional blows can be performed. Ninety-five per cent of untrained healthy subjects and patients can reproduce PEF to within  $0.67 \text{ L}\cdot\text{s}^{-1}$  ( $40 \text{ L}\cdot\text{min}^{-1}$ ), and 90% to within  $0.5 \text{ L}\cdot\text{s}^{-1}$  ( $30 \text{ L}\cdot\text{min}^{-1}$ ) [48]. If satisfactory repeatability has not been achieved in five attempts, more are not likely to be helpful [51].

**Test result selection**

The largest value from at least three acceptable blows is recorded.

**MAXIMUM VOLUNTARY VENTILATION**

This test has been largely superseded by FEV<sub>1</sub>, which was defined as the index from a single maximum forced expiratory manoeuvre that best correlated with maximum voluntary ventilation (MVV). If FEV<sub>1</sub> is available, then MVV has little additional contribution to make in a clinical setting. However, it may be useful in those conditions where ventilatory capacity may be impaired by mechanisms that are different from those affecting FEV<sub>1</sub> [26].

**Definition**

The MVV is the maximum volume of air a subject can breathe over a specified period of time (12 s for normal subjects). It is expressed in  $\text{L}\cdot\text{min}^{-1}$  at BTPS.

**Equipment**

A spirometer used for measuring MVV must have an amplitude–frequency response that is flat ( $\pm 10\%$ ) from zero to  $\geq 4 \text{ Hz}$ , at flows of up to  $12 \text{ L}\cdot\text{s}^{-1}$ , over the volume range. The time for exhaled volume integration or recording must be no less than 12 s and no more than 15 s [52]. The indicated time must be accurate to within  $\pm 3\%$ . The MVV must be measured with an accuracy of  $\pm 10\%$  of reading or  $\pm 15 \text{ L}\cdot\text{min}^{-1}$ , whichever is greater.

The evaluation of equipment is covered in the *Test signals for MVV testing* section.

**Test procedure**

The technician should provide proper instructions and demonstrate the manoeuvre prior to the start of testing. The subject should be tested in the sitting position wearing a nose clip. After the subject makes an airtight seal around the mouthpiece, at least three resting tidal breaths should be obtained, followed by breathing as rapidly and deeply as possible. The tongue and teeth must be positioned so as to not obstruct airflow. The technician should enthusiastically coach the subject throughout the manoeuvre, and may need to suggest faster or slower breathing to achieve an ideal rate of  $90\text{--}110 \text{ breaths}\cdot\text{min}^{-1}$  [53, 54], although subjects with disease may not always achieve this rate. The technician will need to carefully observe the subject with occasional

glances at the tracing to help the subject to obtain an acceptable manoeuvre. An acceptable manoeuvre should be performed with maximal effort without evidence of leakage, hesitation or measurement artefact. The subject is instructed to breathe as deeply and rapidly as possible and the tidal volume ( $V_T$ ) during the manoeuvre should be greater than the subject's resting  $V_T$ .

The test interval (e.g. 12 s) should be reported. A rest between manoeuvres will improve subsequent efforts.

The MVV should be calculated from the sum of all individual exhalations, multiplied by the appropriate BTPS correction factor during the best 12 s of the manoeuvre. From a technical standpoint, changes in respiratory rate or  $V_T$  during the manoeuvre will influence test results.

**Within-manoeuve evaluation**

In normal subjects, the goal for an acceptable MVV should be a  $V_T$  that is  $\sim 50\%$  of the VC, with a breathing frequency that is  $\sim 90 \text{ breaths}\cdot\text{min}^{-1}$  [54]. It is unlikely that an acceptable manoeuvre will be obtained when the breathing frequency is  $< 65 \text{ breaths}\cdot\text{min}^{-1}$  [54]. However, since there are little data on MVV acceptability criteria, no specific breathing frequency or volume is required. The emphasis should be on maximal effort with a goal of  $90 \text{ breaths}\cdot\text{min}^{-1}$  and a volume representing  $\sim 50\%$  of the VC.  $V_T$  during the manoeuvre is probably not as important as breathing frequency, since patients tend to breathe on the portion of the expiratory curve where air is best moved at a given frequency.

**Between-manoeuve evaluation**

The subject should perform a minimum of two acceptable manoeuvres. There are no clinical studies addressing repeatability; however, additional trials should be considered when the variability between acceptable manoeuvres exceeds 20%.

**Test result selection**

The highest acceptable MVV ( $\text{L}\cdot\text{min}^{-1}$  BTPS) and MVV rate ( $\text{breaths}\cdot\text{min}^{-1}$ ) should be reported. An  $\text{MVV}/(40 \times \text{FEV}_1) < 0.80$  indicates that the MVV is low relative to the FEV<sub>1</sub>, and suggests disease or poor effort. Volume *versus* time tracings from at least two acceptable manoeuvres should be retained and available for inspection.

**TECHNICAL CONSIDERATIONS****Minimal recommendations for spirometry systems**

Accurate results require accurate equipment. Spirometer equipment recommendations apply to all spirometers and are minimal requirements. In some circumstances, it may be appropriate to exceed these requirements (i.e. in some research/surveillance applications). Instrumentation recommendations should be followed to provide accurate spirometric data and information that is comparable from laboratory to laboratory and from one time period to another [1]. The accuracy of a spirometry system depends on characteristics of the entire system, from the volume or flow transducer and the use of an in-line filter, to the recorder, display or processor. Changes in any aspect of the equipment or errors at any step in the process can affect the accuracy of the results. For example, if the BTPS correction factor is wrong, an accurately measured FVC will be incorrectly reported.

Spirometers and PEF meters are not required to measure all of the indices in table 6, but must meet the recommendations for those that are measured. Accuracy and repeatability recommendations apply over the entire volume range of the instrument.

### BTPS correction

All spirometry values should be reported at BTPS by any method (measuring temperature and barometric pressure) proven effective by the manufacturer. For volume-type spirometers, the temperature inside the spirometer should be measured for each breathing manoeuvre. Regardless of the BTPS correction technique used, the ambient temperature must always be recorded with an accuracy of  $\pm 1^\circ\text{C}$ . In situations where the ambient air temperature is changing rapidly ( $>3^\circ\text{C}$  in  $<30$  min), continuous temperature corrections may be necessary. Spirometer users should be aware of potential problems with testing performed at lower ambient temperatures:  $17^\circ\text{C}$  is the lower limit [55–63] for ambient temperature, unless a manufacturer states that their spirometer will operate accurately at lower ambient temperatures. If barometric pressure is not used in calculating the BTPS correction factor, the range of barometric pressures over which the BTPS correction factor is valid must be published by the manufacturer.

### Comments

The rationale for this recommendation is based, in part, on the problems with finite cooling times of gases in volume-type spirometers [55–57] and the problems of estimating BTPS

correction factors for flow devices [58–60]. When a subject performs an FVC manoeuvre, the air leaving the lungs is  $\sim 33$ – $35^\circ\text{C}$  [61, 62] and saturated with water vapour. If the expired gas is assumed to be at BTPS, an error of  $\sim 1\%$  will result. Most volume-type spirometers assume instantaneous cooling of the air as it enters the spirometer. This is not always the case, and FEV<sub>t</sub> can be incorrectly reported because of it. For capillary and screen pneumotachometers, the signal depends on gas viscosity, which increases with increasing temperature. Therefore, for pneumotachometers, a different correction factor is needed for recording patients as compared with recording from the calibrating syringe. Also, correction factors will be different for inspiratory and expiratory manoeuvres. It is usually assumed that expired gas does not cool as it passes through the flow sensor. This may not be the case, particularly with unheated flow sensors [58, 59]. The error will increase if the flow sensor is located further from the mouth and more cooling occurs, as is the case when a filter is placed in front of the flow sensor. Water condensation within or on the surfaces of a flow sensor may alter its calibration.

Depending on environmental temperature, the BTPS correction factor may be as large as 10%. The method used to calculate or estimate the BTPS factor can potentially introduce significant errors; examples and a fuller explanation can be found elsewhere [3, 4].

Changes in spirometer temperature can be a source of variability. Spirometer temperature should be measured and not assumed to be constant, even over the course of one testing

**TABLE 6** Range and accuracy recommendations specified for forced expiratory manoeuvres

Test	Range/accuracy (BTPS)	Flow range $\text{L}\cdot\text{s}^{-1}$	Time s	Resistance and back pressure	Test signal
<b>VC</b>	0.5–8 L, $\pm 3\%$ of reading or $\pm 0.050$ L, whichever is greater	0–14	30		3-L Calibration syringe
<b>FVC</b>	0.5–8 L, $\pm 3\%$ of reading or $\pm 0.050$ L, whichever is greater	0–14	15	$<1.5 \text{ cmH}_2\text{O}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ ( $0.15 \text{ kPa}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ )	24 ATS waveforms, 3-L Cal Syringe
<b>FEV<sub>1</sub></b>	0.5–8 L, $\pm 3\%$ of reading or $\pm 0.050$ L, whichever is greater	0–14	1	$<1.5 \text{ cmH}_2\text{O}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ ( $0.15 \text{ kPa}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ )	24 ATS waveforms
<b>Time zero</b>	The time point from which all FEV <sub>t</sub> measurements are taken			Back extrapolation	
<b>PEF</b>	Accuracy: $\pm 10\%$ of reading or $\pm 0.30 \text{ L}\cdot\text{s}^{-1}$ ( $20 \text{ L}\cdot\text{min}^{-1}$ ), whichever is greater; repeatability: $\pm 5\%$ of reading or $\pm 0.15 \text{ L}\cdot\text{s}^{-1}$ ( $10 \text{ L}\cdot\text{min}^{-1}$ ), whichever is greater	0–14		Mean resistance at 200, 400, 600 $\text{L}\cdot\text{min}^{-1}$ (3.3, 6.7, 10 $\text{L}\cdot\text{s}^{-1}$ ) must be $<2.5 \text{ cmH}_2\text{O}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ ( $0.25 \text{ kPa}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ )	26 ATS flow waveforms
<b>Instantaneous flows (except PEF)</b>	Accuracy: $\pm 5\%$ of reading or $\pm 0.200 \text{ L}\cdot\text{s}^{-1}$ , whichever is greater	0–14		$<1.5 \text{ cmH}_2\text{O}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ ( $0.15 \text{ kPa}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ )	Data from manufacturers
<b>FEF<sub>25–75%</sub></b>	7.0 $\text{L}\cdot\text{s}^{-1}$ , $\pm 5\%$ of reading or $\pm 0.200 \text{ L}\cdot\text{s}^{-1}$ , whichever is greater	$\pm 14$	15	Same as FEV <sub>1</sub>	24 ATS waveforms
<b>MVV</b>	250 $\text{L}\cdot\text{min}^{-1}$ at V <sub>t</sub> of 2 L within $\pm 10\%$ of reading or $\pm 15 \text{ L}\cdot\text{min}^{-1}$ , whichever is greater	$\pm 14$ ( $\pm 3\%$ )	12–15	$<1.5 \text{ cmH}_2\text{O}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ ( $0.15 \text{ kPa}\cdot\text{L}^{-1}\cdot\text{s}^{-1}$ )	Sine wave pump

BTPS: body temperature and ambient pressure saturated with water vapour; VC: vital capacity; FVC: forced vital capacity; ATS: American Thoracic Society; FEV<sub>1</sub>: forced expiratory volume in one second; FEV<sub>t</sub>: forced expiratory volume in t seconds; PEF: peak expiratory flow; FEF<sub>25–75%</sub>: mean forced expiratory flow between 25% and 75% of FVC; MVV: maximum voluntary ventilation; V<sub>t</sub>: tidal volume.

session. For volume spirometers, errors up to 6% in FEV<sub>1</sub> and FVC can occur if ambient temperature is used instead of internal spirometer temperature [64]. For volume spirometers, the temperature inside the spirometer should be measured for each breathing manoeuvre.

### Test signals for spirometer testing

The diversity of FVC manoeuvres encountered in clinical practice is currently best simulated by the 24 standard volume–time waveforms developed by the ATS [3] and HANKINSON and GARDNER [65]. These waveforms can be used to drive a computer-controlled mechanical syringe, or its equivalent, for testing actual hardware and software [66, 67], or, when put in a digital form, they can evaluate only the software. Computer-controlled mechanical syringes (*i.e.* pump systems) used for validation should be accurate within  $\pm 50$  mL, which is 0.5% of their full range up to 10 L for FVC and FEV<sub>1</sub>. Pump systems may have accuracy values better than this for many profiles, but reproduce less accurately those test profiles with short DTs and RTs to peak flow [68, 69]. The ATS spirometry statement [3] shows the measured values for each of the 24 standard waveforms. On request, the ATS can provide these waveforms in an electronic format. Appropriate corrections for using gas at the ambient temperature and humidity instead of BTPS may need to be made for some mechanical syringe–spirometer combinations.

### Method

A production spirometer is connected to the pump system for testing, orientated as it would be to test human subjects. Connecting tubing must be kept to the minimum (<0.300 L) and must not be distensible. If an in-line filter is required for testing human subjects, one must be included when the instrument is tested. Each of the 24 ATS waveforms is discharged into the spirometer five times under ambient conditions, and all of the readings are recorded.

BTPS conditions are simulated by discharging waveforms 1–4 to the spirometer three times, using air heated to  $37 \pm 1^\circ\text{C}$  and at >98% relative humidity. The time between each of the three tests should be <2 min.

### Accuracy test

The average of the five tests under ambient conditions is compared with the standard value in the following way:

$$\text{Deviation} = \text{average} - \text{standard} \quad (1)$$

$$\text{Percentage deviation} = 100 \times (\text{average} - \text{standard}) / \text{standard} \quad (2)$$

The accuracy validation limits for volumes, which include the waveform-generator inaccuracy, are  $\pm 3.5\%$  of reading or  $\pm 0.100$  L, whichever is greater. An accuracy error occurs if the deviation (for volumes <2.857 L) or percentage deviation (for volumes >2.857 L) exceed these limits. These limits include the allowable inaccuracy of the pump system.

Acceptable spirometer performance is defined as fewer than three accuracy errors for either FVC or FEV<sub>1</sub> across the 24 waveforms (<5% error rate).

The average FVC and FEV<sub>1</sub> values of the three tests simulating BTPS conditions are compared with the standard values. The

validation limits for these tests under BTPS conditions are  $\pm 4.5\%$  or 0.200 L, whichever is the greater, and these limits include the allowable inaccuracy for the pump system.

Acceptable spirometer performance under BTPS conditions is defined as the accuracy requirement being met for all of the four profiles used.

### Repeatability test

The FEV<sub>1</sub> and FVC data from the accuracy test are used to derive the span of the five recordings:

$$\text{Span} = \text{maximum} - \text{minimum} \quad (3)$$

$$\text{Percentage span} = 100 \times \text{span} / \text{average} \quad (4)$$

The repeatability validation limits for the volume measured at ambient conditions are  $\pm 3.5\%$  or  $\pm 0.100$  L, whichever is the greater, and, for BTPS conditions,  $\pm 4.5\%$  or  $\pm 0.200$  L, whichever is the greater. A repeatability error occurs if the span (for volumes <2.857 L at ambient or 4.444 L at BTPS) or percentage span (for volumes above this) exceeds these limits.

Acceptable spirometer performance for repeatability under ambient conditions is defined as fewer than three accuracy errors for either FVC or FEV<sub>1</sub> across the 24 profiles (<5% error rate). For BTPS conditions, the acceptable spirometer performance for repeatability is defined as the accuracy requirement being met for all of the four profiles.

### Test signals for PEF meter testing

The 26 flow–time ATS waveforms were chosen to represent a range of PEF profiles suitable for delivery by mechanical syringe or pump systems to test PEF meters [3]. The range of profiles and method of delivery may need to be revised, as research on PEF measurement continues [45]. The mechanical syringe or suitable pump system used to validate PEF measuring equipment must have an accuracy of  $\pm 2\%$  in delivering PEF. Pump systems may have difficulty meeting this accuracy standard for profiles more demanding than the set of 26 [68, 69]. Recent evidence suggests that the frequency content in the first second of the blow that contributes to PEF is higher [47] than previously determined [70, 71]. The 26 waveforms may not cover the range of RT and DT found in ~25% of the client population [72], and, hence, more demanding test profiles may be required in future [45].

### Method

Two randomly chosen production models of the flow meters should each have the 26 waveforms delivered to them five times under ambient conditions and the readings recorded. Any waveforms with a PEF outside the meter's stated operational range would not be included in the testing sequence. Appropriate correction factors for testing under ambient conditions should be applied as recommended by the manufacturer.

### Accuracy test

The average reading for each of the two meters is compared with the standard, as for volumes.

The accuracy validation limits are  $\pm 12\%$  or  $\pm 25$  L·min<sup>-1</sup>, whichever is the larger, and these limits include the 2% inaccuracy limit for the waveform generator. An accuracy error

for a given meter and given waveform occurs if the deviation and percentage deviation exceed these limits.

Acceptable performance is defined as fewer than three accuracy errors out of the total of 52 tests (26 waveforms, two meters).

#### Repeatability test

Flow waveforms 1, 4, 8 and 25 are discharged three times to each of 10 production meters. The repeatability validation limits are  $\pm 6\%$  or  $\pm 15 \text{ L}\cdot\text{min}^{-1}$ , whichever is the greater, and these limits include 1% for waveform-generator variability. A repeatability error occurs if the span and percentage span exceed these limits.

Acceptable performance is defined as six or fewer errors in the 120 tests (*i.e.* maximum error rate of 5%).

#### Test signals for MVV testing

A spirometry system used to measure MVV should be tested under ambient conditions with a pump producing a sinusoidal waveform, with stroke volumes up to 2 L using the four patterns of delivery previously specified [3]. Testing at BTPS is not required, and each pattern is tested twice. The accuracy validation limits of the spirometer used for measuring MVV with flows up to  $250 \text{ L}\cdot\text{min}^{-1}$  are  $\pm 10.5\%$  of reading or  $\pm 20 \text{ L}\cdot\text{min}^{-1}$ , whichever is greater. The pressure at the mouthpiece must not exceed  $\pm 10 \text{ cmH}_2\text{O}$  (1 kPa) at any point during MVV testing. These requirements apply to volume spirometers throughout their volume range.

Acceptable performance is defined as no errors in the eight tests (four patterns, twice).

#### ABBREVIATIONS

Table 7 contains a list of abbreviations and their meanings, which will be used in this series of Task Force reports.

TABLE 7 List of abbreviations and meanings	
<b>ATPD</b>	Ambient temperature, ambient pressure, and dry
<b>ATPS</b>	Ambient temperature and pressure saturated with water vapour
<b>BTPS</b>	Body temperature ( <i>i.e.</i> 37°C), ambient pressure, saturated with water vapour
<b>C</b>	Centigrade
<b>CFC</b>	Chlorofluorocarbons
<b>cm</b>	Centimetres
<b>COHb</b>	Carboxyhaemoglobin
<b>DL<sub>co</sub></b>	Diffusing capacity for the lungs measured using carbon monoxide, also known as transfer factor
<b>DL<sub>co</sub>/VA</b>	Diffusing capacity for carbon monoxide per unit of alveolar volume, also known as K <sub>co</sub>
<b>DM</b>	Membrane-diffusing capacity
<b>DT</b>	Dwell time of flow >90% of PEF
<b>EFL</b>	Expiratory flow limitation
<b>ERV</b>	Expiratory reserve volume
<b>EV</b>	Back extrapolated volume
<b>EVC</b>	Expiratory vital capacity
<b>FA<sub>x</sub></b>	Fraction of gas X in the alveolar gas
<b>FA<sub>x,t</sub></b>	Alveolar fraction of gas X at time t
<b>FEF<sub>25-75%</sub></b>	Mean forced expiratory flow between 25% and 75% of FVC
<b>FEF<sub>x%</sub></b>	Instantaneous forced expiratory flow when X% of the FVC has been expired

TABLE 7 (Continued)	
<b>FEV<sub>1</sub></b>	Forced expiratory volume in one second
<b>FEV<sub>t</sub></b>	Forced expiratory volume in t seconds
<b>FE<sub>x</sub></b>	Fraction of expired gas X
<b>FIF<sub>x%</sub></b>	Instantaneous forced inspiratory flow at the point where X% of the FVC has been inspired
<b>Fi<sub>x</sub></b>	Fraction of inspired gas X
<b>FIVC</b>	Forced inspiratory vital capacity
<b>FRC</b>	Functional residual capacity
<b>FVC</b>	Forced vital capacity
<b>H<sub>2</sub>O</b>	Water
<b>Hb</b>	Haemoglobin
<b>Hg</b>	Mercury
<b>Hz</b>	Hertz; cycles per second
<b>IC</b>	Inspiratory capacity
<b>IVC</b>	Inspiratory vital capacity
<b>K<sub>co</sub></b>	Transfer coefficient of the lung ( <i>i.e.</i> DL <sub>co</sub> /VA)
<b>kg</b>	Kilograms
<b>kPa</b>	Kilopascals
<b>L</b>	Litres
<b>L·min<sup>-1</sup></b>	Litres per minute
<b>L·s<sup>-1</sup></b>	Litres per second
<b>lb</b>	Pounds weight
<b>MEF<sub>x%</sub></b>	Maximal instantaneous forced expiratory flow where X% of the FVC remains to be expired
<b>MFVL</b>	Maximum flow–volume loop
<b>mg</b>	Milligrams
<b>MIF</b>	Maximal inspiratory flow
<b>mL</b>	Millilitres
<b>mm</b>	Millimetres
<b>MMEF</b>	Maximum mid-expiratory flow
<b>ms</b>	Milliseconds
<b>MVV</b>	Maximum voluntary ventilation
<b>PA<sub>o2</sub></b>	Alveolar oxygen partial pressure
<b>PB</b>	Barometric pressure
<b>PEF</b>	Peak expiratory flow
<b>P<sub>H2O</sub></b>	Water vapour partial pressure
<b>P<sub>iO2</sub></b>	Inspired oxygen partial pressure
<b>θ (theta)</b>	Specific uptake of CO by the blood
<b>RT</b>	Rise time from 10% to 90% of PEF
<b>RV</b>	Residual volume
<b>s</b>	Seconds
<b>STPD</b>	Standard temperature (273 K, 0°C), pressure (101.3 kPa, 760 mmHg) and dry
<b>TB</b>	Tuberculosis
<b>TGV (or V<sub>TG</sub>)</b>	Thoracic gas volume
<b>t<sub>i</sub></b>	Time taken for inspiration
<b>TLC</b>	Total lung capacity
<b>Tr</b>	Tracer gas
<b>t<sub>tot</sub></b>	Total time of respiratory cycle
<b>V<sub>A</sub></b>	Alveolar volume
<b>V<sub>A,eff</sub></b>	Effective alveolar volume
<b>VC</b>	Vital capacity
<b>V<sub>c</sub></b>	Pulmonary capillary blood volume
<b>V<sub>D</sub></b>	Dead space volume
<b>V<sub>I</sub></b>	Inspired volume
<b>V<sub>S</sub></b>	Volume of the expired sample gas
<b>µg</b>	Micrograms



## APPENDIX

**Proposal for a standard data format for spirometry**

This proposal would not preclude the use of other data formats, but would require that a spirometer should at least be able to output data in the required format. The advantage of a standard format is the ease of moving data into data repositories, such as quality control, healthcare and research databases. It should simplify and reduce the cost of data transfer when users change instrument models and manufacturers. Easier transfer of data into healthcare databases has the potential for improving the utility of lung function by making more complete data readily available to clinicians and healthcare researchers. In research and clinical settings, a standard data format should simplify and reduce the cost of transferring data into quality control software and could contribute to improved overall test quality. Finally, it is time for this change; pulmonary function is one of the last medical arenas without a standard data format.

**Proposed format**

The spirometry data file will consist of an American Standard Code for Information Interchange, comma-delineated file with variable length records. Comma-delineated text files are easily generated and are standard import formats for several database programs. Although some redundancies will exist, each record shall represent one curve and will be terminated with a carriage return and line feed. The ATS will distribute examples of this data format from their web site.

Table 8 shows a list of parameters that must be included in every record. If a parameter is unavailable, the space must remain blank (“,”). The flow–time data points must be provided with a sampling interval of 0.01 s (100 samples·s<sup>-1</sup>) in mL·s<sup>-1</sup>. If necessary, interpolation or other techniques must

**TABLE 8** List of parameters<sup>#</sup>

ID (patient identification)
Patient name
Data type (SP followed by E=expiratory or I=Inspiratory, followed by S=single or B=best curve)
Barometric pressure (mmHg)
Temperature (°C) used in BTPS calculation
Relative humidity (%)
FVC quality attribute (A, B, C, D or F)
FEV <sub>1</sub> quality attribute (A, B, C, D or F)
Effort attribute (A, B, C, D or F)
Interpretation code (see ATS interpretation scheme)
Deleted manoeuvre (Y or N)
Acceptable manoeuvre (Y or N)
Technician quality control code (A, B, C, D or F)
Computer quality code (A, B, C, D or F)
Plateau achieved (Y or N)
Review (N or R for “needs review” or “was reviewed”)
Date of review (DD/MM/YYYY)
Reviewer initials
BTPS factor (x.xxx)
Spirometer manufacturer
Spirometer model
Spirometer serial number
Spirometer type

**TABLE 8** (Continued)

Testing facility name
City
State/region
Zip/post code
Country
E-mail
Phone number
Calibration date (DD/MM/YYYY)
Calibration time (HH:MM)
Calibration result (P or F for “passed” or “failed”)
Date (DD/MM/YYYY)
Time (HH:MM)
Technician ID (technician identification code or initials)
Manoeuvre number
Age (integer years)
Height (cm)
Weight (kg)
Sex (M or F)
Race (2-character race code)
Date of birth (DD/MM/YYYY)
Reference values source (first author surname and date of publication, e.g. “Knudson 1983”)
Reference values correction factor (x.xx, 1.00 for no correction)
Testing position (standing, sitting or supine)
Test type (pre-, post-, bronchodilator, methacholine concentration or dose)
FVC (mL)
Extrapolated volume (mL)
FEV <sub>1</sub> (mL)
FEV <sub>6</sub> (mL)
PEF (mL·s <sup>-1</sup> )
FEF <sub>25–75%</sub> (mL·s <sup>-1</sup> )
VC (mL)
Forced expiratory time (s)
Time to PEF (ms)
Predicted FVC (mL)
Predicted FEV <sub>1</sub> (mL)
Predicted FEV <sub>6</sub> (mL)
Predicted FEV <sub>1</sub> /FVC% (xxx.x%)
Predicted FEV <sub>1</sub> /FEV <sub>6</sub> % (xxx.x%)
Comments text
Original sampling interval (ms)
Blank 1 or FEF <sub>25%</sub>
Blank 2 or FEF <sub>50%</sub>
Blank 3 or FEF <sub>75%</sub>
Blank 4 or FEF <sub>90%</sub>
Blank 5
Blank 6
Blank 7
Blank 8
Blank 9
Blank 10
Number of data points
Flow data points (mL·s <sup>-1</sup> ; variable number contained in number of data points)
Carriage return
Line feed

<sup>#</sup>: All text type variables should be enclosed with double quotes (“”) to prevent confusion with control or data separator type characteristics.

be used to provide the 0.01-s sampling interval. The record length will vary, depending on the number of data points present in the flow-time portions of the record. The curve data must include  $\geq 0.25$  s of data points prior to the onset of the inspiratory or expiratory manoeuvre.

Volume-time curves may be calculated by adding the flow-time values ( $\text{mL}\cdot\text{s}^{-1}$ ) and multiplying the sum by 0.01 s. To obtain the highest precision, the sum of the flow values should be calculated for each volume data point before multiplying by 0.01 s.

#### ACKNOWLEDGEMENTS

M.R. Miller: University Hospital Birmingham NHS Trust, Birmingham, UK; J. Hankinson: Hankinson Consulting, Inc., Valdosta, GA, USA; V. Brusasco: Università degli Studi di Genova, Genova, Italy; F. Burgos: Hospital Clinic Villarreal, Barcelona, Spain; R. Casaburi: Harbor UCLA Medical Center, Torrance, CA, USA; A. Coates: Hospital for Sick Children, Toronto, ON, Canada; R. Crapo and R. Jensen: LDS Hospital, Salt Lake City, UT, USA; P. Enright: 4460 E Ina Rd, Tucson, AZ, USA; C.P.M. van der Grinten: University Hospital of Maastricht, Maastricht, the Netherlands; P. Gustafsson: Queen Silvias Children's Hospital, Goteborg, Sweden; D.C. Johnson: Massachusetts General Hospital and Harvard Medical School, Boston, MA, USA; N. MacIntyre: Duke University Medical Center, Durham, NC, USA; R. McKay: Occupational Medicine, Cincinnati, OH, USA; D. Navajas: Universitat de Barcelona - IDIBAPS, Barcelona, Spain; O.F. Pedersen: University of Aarhus, Aarhus, Denmark; R. Pellegrino: Azienda Ospedaliera S. Croce e Carle, Cuneo, Italy; G. Viegi: CNR Institute of Clinical Physiology, Pisa, Italy; J. Wagner: Pharmaceutical Research Associates, Inc., Lenexa, KS, USA.

#### REFERENCES

- Renzetti AD Jr. Standardization of spirometry. *Am Rev Respir Dis* 1979; 119: 831–838.
- American Thoracic Society. Standardization of spirometry: 1987 update. *Am Rev Respir Dis* 1987; 136: 1285–1298.
- American Thoracic Society. Standardization of spirometry, 1994 update. *Am J Respir Crit Care Med* 1995; 152: 1107–1136.
- Quanjer PH, ed. Standardized lung function testing. Report Working Party Standardization of Lung Function Tests. European Community for Coal and Steel. *Bull Eur Physiopathol Respir* 1983; 19: Suppl. 5, 1–95.
- Quanjer PH, Tammeling GJ, Cotes JE, Pedersen OF, Peslin R, Yernault J-C. Lung volume and forced ventilatory flows. Report Working Party Standardization of Lung Function Tests, European Community for Steel and Coal. Official Statement of the European Respiratory Society. *Eur Respir J* 1993; 6: Suppl. 16, 5–40.
- Morgan KC. The assessment of ventilatory capacity (committee recommendations). *Chest* 1975; 67: 95–97.
- Gardner RM, Crapo RO, Billings RG, Shigeoka JW, Hankinson JL. Spirometry: what paper speed? *Chest* 1983; 84: 161–165.
- Gardner RM, Clausen JL, Crapo RO, et al. Quality assurance in pulmonary function laboratories. *Am Rev Respir Dis* 1986; 134: 626–627.
- Morris AH, Kanner RE, Crapo RO, Gardner RM. Clinical pulmonary function testing: a manual of uniform laboratory procedures. 2nd Edn. Salt Lake City, UT, Intermountain Thoracic Society, 1984.
- Townsend MC. The effects of leaks in spirometers on measurement of pulmonary function. *J Occup Med* 1984; 26: 835–841.
- Association for the Advancement of Medical Instrumentation, Standard for spirometers (draft), October 1980. AAMI Suite 602, 1901 N. Ft. Myer Drive, Arlington, VA 22209–1699.
- D'Angelo E, Prandi E, Milic-Emili J. Dependence of maximal flow-volume curves on time course of preceding inspiration. *J Appl Physiol* 1993; 75: 1155–1159.
- Stoller JK, Basheda S, Laskowski D, Goormastic M, McCarthy K. Trial of standard versus modified expiration to achieve end-of-test spirometry criteria. *Am Rev Respir Dis* 1993; 148: 275–280.
- Bucca CB, Carossa S, Colagrande P, et al. Effect of edentulism on spirometric tests. *Am J Respir Crit Care Med* 2001; 163: 1018–1020.
- Eigen H, Bieler H, Grant D, et al. Spirometric pulmonary function in healthy preschool children. *Am J Respir Crit Care Med* 2001; 163: 619–623.
- Smith AA, Gaensler EA. Timing of forced expiratory volume in one second. *Am Rev Respir Dis* 1975; 112: 882–885.
- Horvath EP Jr, ed. Manual of spirometry in occupational medicine. Division of Training and Manpower Development, National Institutes for Occupational Safety and Health. Cincinnati, NIOSH, 1981.
- Hankinson JL, Gardner RM. Standard waveforms for spirometer testing. *Am Rev Respir Dis* 1982; 126: 362–364.
- Aurora P, Stocks J, Oliver C, et al. Quality control for spirometry in preschoolchildren with and without lung disease. *Am J Crit Care Med* 2004; 169: 1152–1159.
- Desmond KJ, Allen PD, Demizio DL, Kovesi T, Coates AL. Redefining end of test (EOT) criteria for pulmonary function testing in children. *Am J Respir Crit Care Med* 1997; 156: 542–545.
- Hankinson JL, Bang KM. Acceptability and reproducibility criteria of the American Thoracic Society as observed in a sample of the general population. *Am Rev Respir Dis* 1991; 143: 516–521.
- Ferris BG Jr, Speizer FE, Bishop Y, Prang G, Weener J. Spirometry for an epidemiologic study: deriving optimum summary statistics for each subject. *Bull Eur Physiopathol Respir* 1978; 14: 146–166.
- Kanner RE, Schenker MB, Munoz A, Speizer FE. Spirometry in children: methodology for obtaining optimal results for clinical and epidemiological studies. *Am Rev Respir Dis* 1983; 127: 720–724.
- Swanney MP, Jensen RL, Crichton DA, Beckert LE, Cardno LA, Crapo RO. FEV(6) is an acceptable surrogate for FVC in the spirometric diagnosis of airway obstruction and restriction. *Am J Respir Crit Care Med* 2000; 162: 917–919.
- Paoletti P, Pistelli G, Fazzi P, et al. Reference values for vital capacity and flow-volume curves from a general population study. *Bull Eur Physiopathol Respir* 1986; 22: 451–459.

- 26 Pellegrino R, Viegi G, Enright P, *et al.* Interpretative strategies for lung function tests. *Eur Respir J* 2005 (In press).
- 27 Coates AL, Allen PD, MacNeish CF, Ho SL, Lands LC. Effect of size and disease on expected deposition of drugs administered using jet nebulization in children with cystic fibrosis. *Chest* 2001; 119: 1123–1130.
- 28 Coates AL, Ho SL. Drug administration by jet nebulization. *Pediatr Pulmonol* 1998; 26: 412–423.
- 29 Newman SP, Clark AR, Talaee N, Clark SW. Pressurized aerosol deposition in the human lung with and without an “open” spacer device. *Thorax* 1989; 44: 706–710.
- 30 Tal A, Golan H, Grauer N, Aviram M, Albin D, Quastel MR. Deposition pattern of radiolabeled salbutamol inhaled from a meter-dose inhaler by means of a spacer with mask in young children with airway obstruction. *J Pediatr* 1996; 128: 479–484.
- 31 Newhouse MT. Asthma therapy with aerosols: are nebulizers obsolete? A continuing controversy. *J Pediatr* 1999; 135: 5–8.
- 32 Coates AL, MacNeish CF, Lands LC, Meisner D, Kelemen S, Vadas EB. A comparison of the availability of tobramycin for inhalation from vented *versus* unvented nebulizers. *Chest* 1998; 113: 951–956.
- 33 Devadason SG, Everard ML, Linto JM, LeSouëf PN. Comparison of drug delivery from conventional *versus* “Venturi” nebulizers. *Eur Respir J* 1997; 10: 2479–2483.
- 34 Leach CL, Davidson PJ, Hasselquist BE, Boudreau RJ. Lung deposition of hydrofluoroalkane-134a beclomethasone is greater than that of chlorofluorocarbon fluticasone and chlorofluorocarbon beclomethasone: a cross-over study in healthy volunteers. *Chest* 2002; 122: 510–516.
- 35 Wildhaber JH, Devadason SG, Hayden MJ, Elber E, Summers QA, LeSouëf PN. Aerosol delivery to wheezy infants: a comparison between a nebulizer and two small volume spacers. *Pediatr Pulmonol* 1997; 23: 212–216.
- 36 Guidelines for the measurement of respiratory function. Recommendations of the British Thoracic Society and the Association of Respiratory Technicians and Physiologists. *Respir Med* 1994; 88: 165–194.
- 37 Babb TG, Viggiano R, Hurley B, Staats B, Rodarte JR. Effect of mild-to-moderate airflow limitation on exercise capacity. *J Appl Physiol* 1991; 70: 223–230.
- 38 O’Donnell DE, Lam M, Webb KA. Spirometric correlates of improvement in exercise performance after cholinergic therapy in chronic obstructive pulmonary disease. *Am J Respir Crit Care Med* 1999; 160: 542–549.
- 39 Pellegrino R, Rodarte JR, Brusasco V. Assessing the reversibility of airway obstruction. *Chest* 1998; 114: 1607–1612.
- 40 Pellegrino R, Brusasco V. Lung hyperinflation and flow limitation in chronic airway obstruction. *Eur Respir J* 1997; 10: 543–549.
- 41 Younes M, Kivinen G. Respiratory mechanics and breathing pattern during and following maximal exercise. *J Appl Physiol* 1984; 57: 1773–1782.
- 42 Wanger J, Clausen JL, Coates A, Pedersen OF. Standardisation of the measurement of lung volumes. *Eur Respir J* 2005; (In press).
- 43 Brusasco V, Pellegrino R, Rodarte JR. Vital capacities during acute and chronic bronchoconstriction: dependence on flow and volume histories. *Eur Respir J* 1997; 10: 1316–1320.
- 44 Hansen LM, Pedersen OF, Lyager S, Naerra N. [Differences in vital capacity due to the methods employed]. *Ugerkr Laeger* 1983; 145: 2752–2756.
- 45 Miller MR, Atkins P, Pedersen OF. Inadequate peak expiratory flow meter characteristics detected by a computerised explosive decompression device. *Thorax* 2003; 58: 411–416.
- 46 Quanjer PH, Lebowitz MD, Gregg I, Miller MR, Pedersen OF. Peak expiratory flow: conclusions and recommendations of the European Respiratory Society. *Eur Respir J* 1997; 10: Suppl. 24, 2s–8s.
- 47 Miller MR, Lloyd J, Bright P. Recording flow in the first second of a maximal forced expiratory manoeuvre: influence of frequency content. *Eur Respir J* 2002; 19: 530–533.
- 48 Pedersen OF, Rasmussen TR, Omland Ø, Sigsgaard T, Quanjer PH, Miller MR. Peak expiratory flow and the resistance of the mini-Wright peak flow meter. *Eur Respir J* 1996; 9: 828–833.
- 49 Pedersen OF, Pedersen TF, Miller MR. Gas compression in lungs decreases peak expiratory flow depending on resistance of peak flow meter. *J Appl Physiol* 1997; 83: 1517–1521.
- 50 Kano S, Burton DL, Lanteri CJ, Sly PD. Determination of peak expiratory flow. *Eur Respir J* 1993; 6: 1347–1352.
- 51 Ferris BG Jr, Speizer FE, Bishop Y, *et al.* Spirometry for an epidemiologic study: deriving optimum summary statistics for each subject. *Bull Eur Physiopathol Respir* 1978; 14: 145–166.
- 52 Federal Register, 38:4265, Feb. 12, 1973, Section of pulmonary function specifications. Washington, DC, United States Government Printing Office.
- 53 Bernstein L. The effect of the rate of breathing on maximum breathing capacity determined with a new spirometer. *Thorax* 1952; 7: 255–262.
- 54 Miller WF, Johnson RL Jr, Wu N. Relationships between maximal breathing capacity and timed expiratory capacities. *J Appl Physiol* 1959; 14: 510–516.
- 55 Hankinson JL, Viola JO. Dynamic BTPS correction factors for spirometric data. *J Appl Physiol* 1983; 44: 1354–1360.
- 56 Hankinson JL, Castellan RM, Kinsley KB, Keimig DG. Effects of spirometer temperature on FEV1 shift changes. *J Occup Med* 1986; 28: 1222–1225.
- 57 Pincock AC, Miller MR. The effect of temperature on recording spiograms. *Am Rev Respir Dis* 1983; 128: 894–898.
- 58 Hankinson JL, Viola JO, Petsonk EL, Ebeling TR. BTPS correction for ceramic flow sensors. *Chest* 1994; 105: 1481–1486.
- 59 Miller MR, Pincock AC. Linearity and temperature control of the Fleisch pneumotachograph. *J Appl Physiol* 1986; 60: 710–715.
- 60 Perks WH, Sopwith T, Brown D, Jones CH, Green M. Effects of temperature on Vitalograph spirometer readings. *Thorax* 1983; 38: 592–594.
- 61 Cole P. Recordings of respiratory air temperature. *J Laryngol* 1954; 68: 295–307.
- 62 Madan I, Bright P, Miller MR. Expired air temperature at the mouth during a maximal forced expiratory manoeuvre. *Eur Respir J* 1993; 6: 1556–1562.

- 63** Liese W, Warwick WJ, Cumming G. Water vapour pressure in expired air. *Respiration* 1974; 31: 252–261.
- 64** Johnson LR, Enright PL, Voelker HT, Tashkin DP. Volume spirometers need automated internal temperature sensors. *Am J Respir Crit Care Med* 1994; 150: 1575–1580.
- 65** Hankinson JL, Gardner RM. Standard waveforms for spirometer testing. *Am Rev Respir Dis* 1982; 126: 362–364.
- 66** Nelson SB, Gardner RM, Crapo RO, Jensen RL. Performance evaluation of contemporary spirometers. *Chest* 1990; 97: 288–297.
- 67** Gardner RM, Hankinson JL, West BJ. Evaluating commercially available spirometers. *Am Rev Respir Dis* 1986; 134: 626–627.
- 68** Hankinson JL, Reynolds JS, Das MK, Viola JO. Method to produce American Thoracic Society flow–time waveforms using a mechanical pump. *Eur Respir J* 1997; 10: 690–694.
- 69** Miller MR, Jones B, Xu Y, Pedersen OF, Quanjer PH. Peak expiratory flow profiles delivered by pump systems: limitations due to wave action. *Am J Respir Crit Care Med* 2000; 162: 1887–1896.
- 70** Peslin R, Jardin P, Bohadana A, Hannhart B. Contenu harmonique du signal de débit pendant l'expiration forcée chez l'homme normal [Harmonic content of the flow signal during forced expiration in normal man]. *Bull Eur Physiopath Respir* 1982; 18: 491–500.
- 71** McCall CB, Hyatt RE, Noble FW, Fry DL. Harmonic content of certain respiratory flow phenomena of normal individuals. *J Appl Physiol* 1957; 10: 215–218.
- 72** Miller MR, Pedersen OF, Quanjer PH. The rise and dwell time for peak expiratory flow in patients with and without airflow limitation. *Am J Respir Crit Care Med* 1998; 158: 23–27.